Neural Correlates of Consolidation in Working Memory

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Abstract: Many of our daily activities rely on a brain system called working memory, which implements our ability to encode information for short-term maintenance, possible manipulation, and retrieval. A recent intracranial study of patients performing a paradigmatic working memory task revealed that the maintenance of information involves a distributed network of oscillations in the gamma band (>40 Hz). Using a similar task, we focused on the encoding stage and targeted a process referred to as short-term consolidation, which corresponds to the encoding of novel items in working memory. The paradigm was designed to manipulate the subjects' intention to encode: series of 10 letters were presented, among which only five had to be remembered, as indicated by visual cues preceding or following each letter. During this task we recorded the intracerebral EEG of nine epileptic patients implanted in mesiotemporal structures, perisylvian regions, and prefrontal areas and used time–frequency analysis to search for neural activities simultaneous with the encoding of the letters into working memory. We found such activities in the form of increases of gamma band activity in a set of regions associated with the phonological loop, including the Broca area and the auditory cortex, and in the prefrontal cortex, the pre- and postcentral gyri, the hippocampus, and the fusiform gyrus. *Hum Brain Mapp* 28:183–193, 2007. © 2006 Wiley-Liss, Inc.

Key words: working memory; encoding; gamma band; intracranial EEG

INTRODUCTION

Our ability to store verbal information in the short term is a fundamental element of our everyday life, referred to as verbal working memory [Baddeley, 1992]. Our understanding of the fundamental mechanisms underlying this function depends on precise spatial and temporal studies of the multiple networks

underlying the perception and encoding of verbal information for short-term maintenance and retrieval. Numerous functional imaging studies have identified key brain regions of those networks [Smith and Jonides, 1998], but their dynamics of activation and the neural activity patterns that support their functions are less well understood.

Those last aspects have been addressed recently for the first time in two studies using local electrophysiological recordings in humans [Howard et al., 2003; Raghavachari et al., 2001]. They recorded the intracranial EEG of epileptic patients while they learned a series of letters presented sequentially (the classic Sternberg paradigm) and found that the memory processes were accompanied with widespread energy increases in the theta (4–7 Hz) and gamma band (>40 Hz) EEG. One striking result was that the energy measured in the gamma band increased with the memory

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load, that is, the number of letters already presented and stored in a series.

Those studies extended the conclusions of a large body of literature emphasizing the role of focal gamma oscillations in perception and visual short-term memory [Singer, 1999; Tallon-Baudry and Bertrand, 1999] to support the view that gamma oscillations participate in the perceptual and maintenance stages of working memory. A natural question is whether gamma band activities also play a role in the encoding stage of working memory. If this is the case, then a second question is whether this network can be distinguished from the network of gamma activities mediating perception. Those are the two questions addressed by the present study.

Before addressing those questions, it is important to provide a more specific definition of the type of encoding under study. Jolicoeur and Dell'Acqua [1998] specifically addressed the notion of encoding and distinguished between three types: sensory encoding, perceptual encoding, and short-term consolidation. In that article, sensory encoding was defined as automatic, not subject to interference by other cognitive processes, and as corresponding to the extraction of the sensory features of the stimulus, which can give rise to sensory persistence. Perceptual encoding was defined as the process by which patterns are recognized, and the representation at this stage of encoding contains information about the identity of the patterns (such as the letters) but needs to receive bottom-up input from the sensory systems, otherwise it decays rapidly. Finally, short-term consolidation is defined as the process of encoding information into short-term memory, which is required for verbal report. This work echoed the proposition of Cowan [2001; discussion in Ruchkin et al., 2003] that visual working memory consists of at least three stages: an initial, high capacity, very limited duration iconic store that encodes the physical features of stimuli, an intermediate transient stage, and a limited capacity, postcategorical sustained short-term store. A similar view was also expressed by Potter [1976] and others. Taking into account these distinctions, the type of encoding studied here corresponds to the process of short-term consolidation, that is, the encoding in working memory (and the term "encoding" will be used in that specific sense in the rest of the article).

The main difficulty is to isolate the encoding stage from the perceptual stage, because encoding usually starts as soon as an item is perceived. One way to decouple the two is to introduce a delay between the presentation of the item and the instruction to memorize it, provided that certain items must be ignored [Reber et al., 2002].

We introduced this manipulation in the task used by Howard et al. [2003] to test for the existence of a network of gamma band activations associated with the encoding phase. In this paradigm, performed by nine epileptic patients who underwent intracerebral recordings, letters were presented one by one and followed (in one experimental condition) or preceded (in a second condition) by an instruction to memorize it or not. We assumed that the active

encoding phase started after the presentation of the second stimulus of each instruction-letter pair, and thus shifted between the two conditions from the presentation of the instruction to the presentation of the letter. We found a network of focal gamma activations showing a similar latency shift and distributed in focal centers in the prefrontal cortex (BA 9, 10, 44, 45, 46), the precentral and postcentral gyri, the auditory cortex, the fusiform gyrus, and the hippocampus.

SUBJECTS AND METHODS

Subjects

The 9 patients (P1–P9) suffered from drug-resistant partial epilepsy and were candidates for surgery. There were 5 women and 4 men, ages 21–53 years (mean, 35.7 years). Magnetic resonance imaging (MRI) of the brain showed different types of lesions in 7 cases (hippocampal sclerosis in P1, P3, P8; prefrontal dysembryoplastic neuroepithelial tumor in P7; anterolateral temporal cavernoma in P2; fronto-orbital arachnoidian cyst in P5; and periventricular nodular heterotopia in P4), and was normal in the remaining two patients (P6, P9). Because the location of the epileptic focus could not be identified using noninvasive methods, the patients underwent intracerebral EEG recordings by means of stereotactically implanted multilead depth electrodes (SEEG) (for explanation of this methodology, see Kahane et al. [2004]), on the basis of which the epileptogenic zone proved to be right temporal in two cases (P1, P8), left temporal in two cases (P2, P3), right prefrontal in one case (P7), left insular in one case (P5), and right insulo-temporal in one case (P9). In the remaining two patients, seizures proved to arise from the heterotopia in one (P4), and were not clearly localized in one (P6).

Selection of sites to implant was made entirely for clinical purposes, with no reference to the present experimental protocol; however, patients who entered this protocol were selected because their implantation sampled regions classically associated with verbal working memory. The patients performed the task 4 days after the implantation of the electrodes, and all had previously given informed consent to participate in the experiment.

Electrode Implantation

In all, 11–14 semirigid electrodes were implanted per patient in cortical areas that varied depending on the suspected origin of seizures (Fig. 1). A total of 110 electrodes were implanted in the nine patients, 61 in the right hemisphere and 49 in the left. Each electrode had a diameter of 0.8 mm and comprised 10 or 15 leads of 2 mm length, 1.5 mm apart (Dixi, Besançon, France), depending on the target region. Therefore, various mesial and lateral cortical areas were evaluated, including the sulcal cortex. The electrode contacts were identified on each individual stereotactic scheme and

Figure 1.

Experimental paradigm and recording sites. **a:** Entry points of the intracranial electrodes across all patients, represented on a 3-D reconstruction of the MNI single-subject MRI. The electrodes are rods oriented perpendicular to the plane of the figure. A total of 110 electrodes were implanted, 49 in the left hemisphere (left side of the figure), and 61 in the right hemisphere (right side of the figure). **b:** Experimental paradigm. In the BEFORE condition the subjects had to memorize the five-out-of-ten letters preceded by green dots (the “yes” cues); in the AFTER condition, the subjects had to memorize the five-out-of-ten letters followed by a green dot. Red dots for the patient meant that s/he did not have to memorize the associated letter. Each item (dot or letter) stayed onscreen for 1 s and was immediately replaced by the next item. Memory encoding is expected to start only when the subject has an item to memorize and has been instructed to do so (some degree of automatic encoding may start during the letter presentation in the AFTER condition, but the task does not encourage this, because the letter stays onscreen until the subsequent cue appears). The moment of encoding should therefore shift from the letter onset in the BEFORE condition, to the green-dot/“yes”-cue onset in the AFTER condition. Red arrows point toward the x, y, and z directions in Talairach space. [Color figure can be viewed in the online issue, which is available at www.interscience.wiley.com.]

then anatomically localized using the proportional atlas of Talairach and Tournoux [1988]. In addition, the computer-assisted matching of postimplantation a computerized tomography (CT) scan with a preimplantation 3-D MRI provided a direct visualization of the electrode contacts with respect to the brain anatomy of each patient (Activis, Lyon, France).

Paradigm

The paradigm was a modified version of the task used by Howard et al. [2003]. Subjects were presented with a series of 10 different letters (randomly chosen between A and O), interleaved with 10 central dots, either green (five dots) or red (the remaining five dots) (Fig. 1). The dots served as visual cues instructing the patients to memorize or not the previous (in a condition named AFTER) or subsequent letter (in a condition named BEFORE), and green dots served as “yes” signals (memorize) while red dots served as “no” signals (ignore). Within one experimental block the patients were presented with 10 such series of 10 letters and 10 dots and the condition was kept constant. All series followed the same temporal organization: a white fixation cross would appear for 1 s at the center of the blue computer screen, replaced by a central X-letter that stayed on-screen for 3 s and served both as a fixation point and as an instruction to concentrate. The 10 letters and 10 cues would then alternate, each item being presented for 1 s, immediately followed by the next item. Four seconds after the onset of the last letter the patients would receive a visual instruction (“response?”) to spell out loud the five letters associated with a “yes” cue. Note that this is an important difference from the paradigm used by Howard et al. [2003], introduced to check the actual memory performance of the patients for each series of letters. A new series would then begin a couple of seconds later after a short relaxation period. The protocol included six BEFORE blocks and six AFTER blocks, intermixed, between which the patients could relax and was informed of the nature of the upcoming block (BEFORE or AFTER), and of an estimation of their performance in the last block. Subjects were explicitly instructed to remain silent during the blocks, except when they gave their responses.

All stimuli were shown foveally on a 17” computer screen. The stimulus dimensions were 4×4 cm for the letters and 2×2 cm for the dots, subtending a visual angle of $\sim 1 \times 1^\circ$ and $0.5 \times 0.5^\circ$ at the 200-cm viewing distance.

Recordings

Intracerebral recordings were conducted using an audiovideo EEG monitoring system (Micromed, Treviso, Italy) that allowed the simultaneous recording of 63 depth-EEG channels sampled at 512 Hz (0.1–200 Hz bandwidth) during the experimental paradigm. One of the contact sites in the white matter was chosen as a reference. This reference had the same impedance as the other contact sites, and was located in a region with no or little source of electrical field; in addition, it was not contaminated by eye movement artifacts or electromyographic activity from subtle muscle contractions. However, all signals were re-referenced to their nearest neighbor on the same electrode, 3.5 mm away before analysis (bipolar montage). Recording sites showing clear epileptiform activities were excluded from the analysis, and among the remaining sites monopolar and bipolar data were systematically inspected, both raw and highpass filtered

(above 15 Hz), and any trial showing epileptic spikes in any of those traces was discarded.

Time–Frequency Analysis

For each single trial, bipolar derivations computed between adjacent electrode contacts were analyzed in the time–frequency domain by convolution with complex Gaussian Morlet’s wavelets [Tallon-Baudry et al., 1996], thus providing a time–frequency power map $P(t, f) = |w(t, f) * s(t)|^2$, where $w(t, f)$ was for each time t and frequency f a complex Morlet’s wavelet $w(t, f) = A \exp(-t^2/2\sigma_t^2) \cdot \exp(2i\pi f t)$, with $A = (\sigma_t \pi)^{-1/2}$ and $\sigma_t = 1/(2\pi\sigma_f)$ and σ_f a function of the frequency f : $\sigma_f = f/7$.

For visualization purposes, normalized time–frequency plots were computed for each bipolar derivation. This normalization was done separately for each frequency and consisted of (1) subtracting the mean power during a [–500 ms: –100 ms] prestimulus baseline, and (2) dividing by the standard deviation of the power during this same baseline.

Comparison between pairs of cue/letter combinations (e.g., “yes”-cue/letter vs. “no”/letter) were done via a Kruskal–Wallis nonparametric analysis (chosen because it makes no assumption about the distribution of the data) [Kruskal and Wallis, 1952; Wikipedia, 2006] applied on the raw time–frequency values of energy, on a set of time–frequency tiles [100 ms $\times$ 30 Hz] covering a [0 : 2000 ms] $\times$ [5 : 250 Hz] domain. There was one test per tile comparing the values obtained for all the trials in the two conditions, in total, the [0 : 2000 ms] $\times$ [5 : 250 Hz] time–frequency domain was covered by $39 \times 14 = 546$ [100 ms $\times$ 30 Hz] tiles (considering an overlap of 50% along the time and frequency dimensions). To apply a Bonferroni correction, we set the threshold for significance for each individual test to $P = 0.0001$, which yields a corrected threshold of 0.05 for all the tests. Note that this Bonferroni correction, which assumes that all the tests are independent, was certainly too conservative, since the energy values measured in consecutive tiles were not independent because of the limited time and frequency resolution of the wavelet transform. However, there is no simple way to perform an exact correction, as the correlation between consecutive energy values depends on frequency, as does the temporal and frequency resolution of the wavelet transform.

Electrodes presented in the Results section were selected because they reached the criterion of $P < 0.0001$ in at least one of the time–frequency tiles. However, in this study we did not consider isolated effects, that is, effects found in one brain region in only one patient, but with no equivalent in the other patients. This strategy was used to compensate the limitation imposed by the fact that in a given patient a specific brain region is sampled by only one electrode; therefore, since the reproducibility of an effect cannot be tested across sites in a single patient, we impose that it is compensated by a reproducibility in at least another patient with an electrode in the same functional structure.

EEG signals were evaluated with the software package for electrophysiological analysis (ELAN-Pack) developed in the INSERM U280 laboratory.

RESULTS

The patients were successful at memorizing the letters when instructed to do so by the cue (recall percentage $91.6\% \pm 6.6\%$ for the letters associated with a memorization instruction). We could not systematically test whether the other letters were memorized or not, because any question concerning those “ignored” letters would have brought the patient’s attention to them. However, when we occasionally asked the patients whether they could remember some of the nontarget letters their answer was either that they did not pay attention to them or that our question was weird, since they were instructed to ignore them.

The data analysis compared for each recorded site the energy modulations induced in the gamma band by “yes” vs. “no” cue/letter sequences in a search for cue-related modulations defined as significant energy differences between the two conditions (Kruskal–Wallis test, $P < 0.0001$, see Subjects and Methods); this was done separately in the BEFORE and the AFTER condition.

Figure 2 illustrates the key manipulation of this paradigm. In the BEFORE condition, the cues instructing the patients to memorize or not the associated letters come before the letters, while in the AFTER condition, they come after the letters. Therefore, if we assume that the process of actively encoding a target letter into working memory should start only after both the letter and the memorization instruction (the cue) have been presented (see black frame in Fig. 2c), then cue-related gamma energy modulations should follow this shift and switch between the two conditions from the letter onsets (in the BEFORE condition) to the cue onsets (in the AFTER condition), as they should if associated with the encoding process.

The time–frequency statistical analysis revealed cue-related energy modulations in the gamma band in a subset of the recording sites (17 of 324) (by cue-related modulation, we mean an energy modulation in response to a cue or to a letter that varies with the value of the cue). Those were confined in small anatomical clusters located in the posterior aspect of the prefrontal cortex (BA 44, 46), which corresponds, in the dominant hemisphere for language, to the pars opercularis of Broca area), the precentral and the postcentral gyrus, the auditory cortex, the prefrontal cortex, the fusiform gyrus, and the hippocampus (see Table I for the list of activated sites with their Talairach coordinates). The effects were observed both in the BEFORE and the AFTER conditions; however, the latencies of the effects varied across conditions. In the BEFORE condition the effect was predominantly after the letter: letters preceded by a “yes” cue induced an increase in gamma energy while those preceded by a “no” cue did not (except in the hippocampus, where no increase was observed in this condition). The statistical analysis revealed that the effect typically extended over a wide (40–150 Hz) frequency band and lasted up to several hundreds of milliseconds after the letter presentation, with latencies variable across sites. In the AFTER condition, the effect was observed after the cue presentation and before the letter presentation: “yes” cues induced a gamma energy

Figure 2.

A possible neural correlate of memory encoding in Broca area (pars opercularis). **a:** Time–frequency representation showing the EEG energy modulation induced in Broca area by “yes”-cue/letter pairs in the BEFORE (Bg) and AFTER (Ag) conditions (each time-course is expressed in units of the standard deviation of the [–500 ms : –100 ms] prestimulus period). In all maps the cue occurs at 0 ms and the subsequent letter at 1000 ms (Br) and (Ar): same for “no”-cue/letter pairs. **b:** Statistical time–frequency maps showing the *P*-values of the Kruskal–Wallis comparison between the “yes” cue/letter and “no” cue/letter pairs in the BEFORE (SB) and AFTER (SA) conditions; what we called “cue-related effects” correspond to time–frequency areas with $P < 0.001$. **c:** Schematic

prediction of the moment when memory encoding should start (black frame) in the BEFORE (left) and AFTER (right) conditions. **d:** Time profiles of the average energy in the 40–150 Hz band for each of the maps shown in panel a (Ag, Ar, Bg, Br). **e–f:** Reconstructions on the MNI single-subject MRI of the recording positions in Broca area with cue-related effects in the gamma band (P3, R’8 site, the illustrated example, and P2, R’6 site; see Table I for the Talairach coordinates). All time–frequency maps correspond to the EEG recorded in R’8, the site indicated by the black arrow. [Color figure can be viewed in the online issue, which is available at www.interscience.wiley.com.]

increase while “no” cues did not. Thus, the cue-related gamma energy modulations, when present, followed the predicted latency shift between conditions: as illustrated in Figure 2c, the modulation shifted between the BEFORE condition and the AFTER condition, from the onset of the letter to the onset of the cue, 1 s earlier.

Figures 2–6 illustrate those gamma energy modulations for each anatomical cluster, with the recording sites reconstructed on the Montreal Neurological Institute (MNI) single-subject MRI. In each figure the displays are organized so that the gamma band responses in the four conditions (responses to target and nontarget letters in the BEFORE and AFTER conditions) can be compared in amplitude and in timing. As mentioned above, the effects most clearly associated with encoding are the responses where latency is shifted between the BEFORE (i.e., left column) and AFTER (i.e., right column) conditions. Figure 2 shows the two sites where a cue-related modulation was observed in the Broca area pars opercularis in the left hemisphere, and the time–frequency energy variations

across conditions and memorization instruction for one of those sites. The sharp gamma band energy increase is clearly visible in both conditions, and shifts from the letter onset to the cue onset between the BEFORE and the AFTER condition. Similar effects were observed in two sites in the precentral gyrus, i.e., in regions associated, respectively, with the motor and sensory representation of the face and larynx (Fig. 3). In the auditory cortex (Fig. 4), the shift was observed in four sites from four different patients, two in each hemisphere, and interestingly the effect started slightly later than in the Broca area (compare Figs. 5 and 2). The other sites with an effect were in the prefrontal cortex (two sites, Fig. 5), in the fusiform gyrus (two sites, Fig. 6), and in the hippocampus. The two sites in the fusiform gyrus were located in symmetrical positions in the two hemispheres, in a region close to the proposed Word Form Area [Cohen et al., 2000] (see Table I for Talairach coordinates). In this region of the visual ventral pathway, gamma energy bursts occurred not only

TABLE I. Talairach coordinates for the recording sites with cue-related gamma energy modulations

Anatomical location	Patient	L/R	Talairach coordinates: <i>x, y, z</i>
Broca			
R'6	2	L	-59, 2.1, 14
R'8	3	L	-65, 5.8, 12
Pre/postcentral			
H'12	5	L	-55, -4.3, 37
S'8	3	L	-69, -15, 24
H14	9	R	64, -19, 31
S10	8	R	65, -19, 19
Auditory cortex			
U'7	3	L	-62, -26, 7.8
U'3	2	L	-53, -30, 6.1
W3	7	R	39, -18, 11
X2	1	R	32, -22, 10
Prefrontal			
Q2	9	R	33, 13, 8.3
G'12	6	L	-54, 39, 11
Fusiform gyrus			
E'9	4	L	-51, -51, -12
E'5	1	L	-42, -42, -12
F'8	2	L	-50, -52, -12
Hippocampus			
E'2	3	L	-27, -17, -21
B'3	1	L	-31, -27, -9.3

Each brain region is the object of a specific figure (2 to 6) showing the corresponding recording sites (except for the hippocampus). The coordinates of the sites chosen as illustrative examples in each figure are in bold. Talairach coordinates *x, y, z* of the sites are shown in millimeters. The *x, y, z* values were converted to MNI coordinates only for the purpose of representing the sites onto the MNI single-subject MRI.

in response to the letters but also in response to the cues, and in the BEFORE condition, the energy was stronger for the “yes” cues, in addition to the cue-related modulation of the gamma peak induced by the letter, although the latter effect was broader. Finally, the effect in the hippocampus was atypical and different from the other sites, since cue-related gamma modulations were only observed in the AFTER condition.

DISCUSSION

Working memory involves at least four stages: perceptual and memory encoding, maintenance, and retrieval. Those stages are usually tightly bound together, and most of the studies that have tried to identify their individual neural substrates have acknowledged the difficulty in decoupling them [Manoach et al., 2003]. The purpose of the present study was to single out the memory encoding stage and to correlate it with precisely timed neural events. We believe that we found such correlates in the form of a distributed network of focal gamma band activations, part of which matches relatively well to what has been described as the phonological loop.

Several groups have successfully used functional MRI (fMRI) or PET to identify key brain structures for each of

those four memory stages through intelligent experimental designs and analysis techniques [Manoach et al., 2003; Reber et al., 2002] that managed to decouple them. However, those functional imaging techniques could not resolve the flow of information processing that occurs over time scales on the order of tens of milliseconds [Buckner and Koutstaal, 1998] and they must ultimately be completed by focal electrophysiological studies of those brain structures, which is available only in epileptic patients. Such recordings are necessary (1) to directly measure the absolute and relative latencies of the neural activations within those structures, (2) to follow the quick transition between memory stages, and (3) to associate those stages with actual neural processes [Lachaux et al., 2003].

One of the first studies to investigate verbal working memory at such a fine resolution revealed gamma oscillations whose amplitude covaried with memory load, which is a property characteristic of a neural correlate of the maintenance process [Howard et al., 2003]. The present study

Figure 3.

The same as Figure 2 for the precentral and postcentral recording sites. S10 (in P8) is the example, the other sites are S'8 (P3), H'12 (P5), and H14 (P9) (see Table I for the Talairach coordinates). [Color figure can be viewed in the online issue, which is available at www.interscience.wiley.com.]

Figure 4.

The same as Figure 2 for the recording sites in the auditory cortex. W3 (in P7) is the example shown, the other sites being X2 (P1), U'3 (P2), and U'7 (P3). [Color figure can be viewed in the online issue, which is available at www.interscience.wiley.com.]

shifted the focus of investigation to the encoding phase of verbal working memory, whose neural substrates remain unclear. Our framework draws on recent observations [Fell et al., 2001; Sederberg et al., 2003] showing that the amplitude of the gamma oscillations induced by the presentation of words was predictive of their successful encoding into long-term memory. Although long-term memory and working memory are distinct processes, we hypothesized that the same would be true for verbal working memory.

Our paradigm was based on the logical premise that on average encoding starts when a subject has (1) an item to encode, and (2) the intention to encode it. Note once again that the term “encoding” refers here to the consolidation in working memory, as presented in the Introduction with reference to Jolicoeur and Dell’Acqua [1998] (sensory and perceptual encoding certainly starts as soon as a letter is presented in both the AFTER and BEFORE conditions). Also, we do not claim that all the target letters are encoded while none of the nontarget letters are, since in some instances items that are not to be encoded (nontarget letters) can still be in the form of incidental encoding. What we claim is that

our experimental paradigm created a bias between the two categories of letters, and that the target letters yielded on average a deeper consolidation process than the nontarget letters. This last claim is based on the repeated observation that the memory span for letters is typically below 7 [Cowan, 2001; Miller, 1956]: since the subjects recollected more than 4 of the 5 target letters on average (see Results), it is unlikely that the nontarget letters were memorized as well, because this would have required from the subjects an average memory span above 8.

By presenting first the item or the instruction, we could therefore move in time the moment of the encoding, and we found gamma energy modulations that followed this manipulation. Those gamma modulations may therefore constitute part of the neural substrate of this encoding process. Note that those gamma modulations extended in a broad gamma range, consistent with previous intracranial observations from our group and others [Lachaux et al., 2005; Tanji et al., 2005].

Before going further, we should note a couple of qualifications to our strong conclusions. First, we are fully aware

Figure 5.

The same as Figure 2 for the prefrontal sites. G'12 (in P6) is the example, the other site is Q2 (P9). [Color figure can be viewed in the online issue, which is available at www.interscience.wiley.com.]

Figure 6.

The same as Figure 2 for the sites in the fusiform gyrus. E'5 (in P1) is the example, the other sites being F'8 (P2) and E'9 (P4). [Color figure can be viewed in the online issue, which is available at www.interscience.wiley.com.]

that these results are correlative by nature, as in any functional imaging study, and do not constitute an indisputable proof that encoding requires this network of gamma activations. We should keep in mind, then, that the sampling of brain tissue provided by those implanted electrodes was limited to a small portion of the brain, such that important functional areas involved in memory encoding may not have been explored. Also, we do not claim that those activations are the only neural substrate of the encoding phase, even in this region, as low frequency-evoked potentials may also participate in this function. Further, we cannot exclude the possibility that at least in some cases the difference in memorization between target and nontarget letters occurs not at the level of the encoding, but at a subsequent stage that would include an active forgetting of the nontargets, a phenomenon demonstrated by Anderson et al. [2004]. However, Figure 7, which shows the time course of gamma activity in a frontal site when the five nontarget letters are presented first, seems to contradict this possibility: the graph shows clearly that the change in neural activity occurs solely

in response to the target letters, and not in response to the nontarget letters, as would be expected if it was related to a suppressive mechanism. Finally, although our study focused on the encoding phase, we also observed gamma band activations that increased in power with the memory load (Fig. 7). This confirmed the link established by Howard et al. [2003] between gamma oscillations and the maintenance phase. Together, our two studies support the proposition that gamma activity serves to organize the content of working memory [Jensen and Lisman, 1998].

Nevertheless, to our knowledge our study was the first effort to find correlations between the encoding phase of verbal working memory and direct measures of local neural activities. It is therefore impossible to compare our findings with observations of a similar nature; however, it is tempting to try a comparison with previous functional imaging studies, provided a spatial congruence between the neural phenomena quantified by metabolic measures and gamma band activations (a correspondence between the blood oxygenation level-dependent (BOLD) signal and gamma band activities has received recent support [Logothetis, 2002]). Several of the gamma activations observed in this study were located in brain regions classically associated with speech, such as the Broca area (pars opercularis) and the pre-

Figure 7.

Gamma band energy correlates with memory load in Broca area. We used an additional control condition, similar as BEFORE, except that the patients knew in advance that the five letters to memorize would always be the last ones to be presented. This figure shows the average energy in the 50–150 Hz band across the entire sequence of letters for a recording site located in Broca area (the same site chosen to illustrate Fig. 2). The energy shows a steady increase throughout the five letters to memorize, in addition to rapid bursts at the onset of the letters. Note also the strong increase at the time of the subject's response. [Color figure can be viewed in the online issue, which is available at www.interscience.wiley.com.]

and postcentral sensory-motor representations of the face and larynx. Indeed, all those regions showed a strong gamma activation when the patients gave verbal responses at the end of each series of letters (Fig. 7).

More precisely, the pars opercularis of Broca has been associated with the manipulation of phonology [Fiez, 1997; Jobard et al., 2003], with subvocal rehearsal [Paulesu et al., 1993], and with verbal working memory [Fiez et al., 1996]. The precentral and postcentral gamma activations can be interpreted as sensorimotor activations during articulatory motor sequences subtending subvocalizations, as identified by functional imaging [Fox et al., 1987; Perry et al., 1999]. This strongly suggests that implicit speech has been operative in those patients during the encoding of the letters. This is further confirmed by the fact that gamma activations were observed in the auditory cortex, a structure also activated by subvocalization [Belin et al., 2000; Smith et al., 1995] and auditory imagery [Kraemer et al., 2005]. Also, introspective reports from the subjects suggested that they indeed spelled out the letters mentally.

This anatomical organization is partly consistent with the model of the phonological loop, introduced by Baddeley in an influential model of working memory as “a phonological store, which can hold memory traces for a few seconds before they fade out, and an articulatory rehearsal process that is analogous to subvocal speech” [Baddeley, 2003b: p 830]. The functions performed by the phonological loop are explicitly those necessary to perform the Sternberg task, and our results confirm that the loop may also participate in the encoding of novel items, possibly via an articulatory process that would update the content of the memory store by adding the new item to the list already stored. Our results also confirm that this network is not solely devoted to a continuous articulatory rehearsal, as correctly suggested by Cohen et al. [1997].

Our observations are in line with the previous fMRI studies that have localized components of the phonological loop in the frontal speech areas [Smith and Jonides, 1998]. It is in fact quite remarkable, given that the exact relationship between BOLD and gamma oscillations is still unknown, that the two phenomena tend to gather in the same regions. Note that many fMRI studies have also found activations in the posterior parietal cortex when short-term storage of verbal material was needed [Smith and Jonides, 1998]; however, our electrodes did not sample this region.

Other gamma effects were observed in the prefrontal cortex, the hippocampus, and the fusiform gyrus and are unlikely to directly mediate the phonological loop. The prefrontal cortex has been frequently found to be active during working memory tasks [Cohen et al., 1994; Miller et al., 1996], but in the dorsal lateral prefrontal cortex, which could mediate the manipulation of stored information [Smith and Jonides, 1998] and attention load [Mazoyer et al., 2002]. In the present study the activation sites were more ventral, slightly anterior to Broca, and therefore likely involved in implicit speech. The same is probably not true for the gamma band effects observed in the

hippocampus and the fusiform gyrus. In the hippocampus, cue-related modulations were only observed in the AFTER condition, in response to the cue onset, which may be surprising in light of recent evidence that the gamma oscillations in the hippocampus play a role in the encoding phase, at least for words and in long-term memory [Fell et al., 2001]. We have no straightforward interpretation for this; one should simply note that the AFTER condition is the only one in which the encoding takes place in the absence of the item to encode (in fact, right after it disappears). In our particular protocol, the hippocampus may not be necessary when the item to encode is still physically available to the subject (as in the BEFORE condition).

In the fusiform gyrus the cue-effect had two aspects. In addition to the shift apparent in the other regions, which we associated with the encoding phase, a cue-effect was observed in response to the dots in the BEFORE condition. This effect cannot be attributed to the encoding of the subsequent letter, and must probably be thought of as a visual attention effect, in the light of recent studies showing that visually induced gamma activations in the fusiform gyrus are very sensitive to attentional modulations, particularly in the period preceding the attended stimulus [Tallon-Baudry et al., 2005]. If this interpretation is correct, then this task would bring into play two systems of gamma activations: one for the perception of the items, and modulated by attention, and the other for their encoding into working memory and modulated by the subject's intention to memorize.

This should be emphasized, since it would provide a neural basis for the distinction between two major causes of fluctuations in memory performance: fluctuations in the attention to the items, and fluctuations in the intention to memorize them [Reber et al., 2002]. It is a familiar fact, validated by behavioral experiments [Kensinger et al., 2003; Naveh-Benjamin et al., 2003], that memory suffers from divided attention during learning. And it has been shown that it is most likely the encoding phase that is affected [Iidaka et al., 2000]. However, it is often difficult to dissociate actual perceptual attention modulations from modulations of the subject's intention to memorize [Reber et al., 2002]. Our results suggest that the two phenomena operate on two different systems of gamma activations: one mediating the perception of the verbal information and one mediating the encoding of this information. Fluctuations in the attention to the item certainly correspond to energy fluctuations in the first of those two systems, as supported by several human and animal studies [Fell et al., 2003; Fries et al., 2001], and as confirmed by our observations in the fusiform gyrus [Lachaux et al., 2005]. We provide evidence that the second of those two networks is sensitive to variations in the subject's intention to encode, which can thus be measured quantitatively. Therefore, the monitoring of gamma activity in specific, distributed brain regions may constitute an objective measure of encoding intention and perceptual attention fluctuations during working memory paradigms.

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