Published in final edited form as:

Bull Math Biol. 2017 November ; 79(11): 2672–2695. doi:10.1007/s11538-017-0346-6.

Multiscale modeling of diffusion in a crowded environment

Lina Meinecke*

Department of Information Technology, Uppsala University

Abstract

We present a multiscale approach to model diffusion in a crowded environment and its effect on the reaction rates. Diffusion in biological systems is often modeled by a discrete space jump process in order to capture the inherent noise of biological systems, which becomes important in the low copy number regime. To model diffusion in the crowded cell environment efficiently, we compute the jump rates in this mesoscopic model from local first exit times, which account for the microscopic positions of the crowding molecules, while the diffusing molecules jump on a coarser Cartesian grid. We then extract a macroscopic description from the resulting jump rates, where the excluded volume effect is modeled by a diffusion equation with space dependent diffusion coefficient. The crowding molecules can be of arbitrary shape and size and numerical experiments demonstrate that those factors together with the size of the diffusing molecule play a crucial role on the magnitude of the decrease in diffusive motion. When correcting the reaction rates for the altered diffusion we can show that molecular crowding either enhances or inhibits chemical reactions depending on local fluctuations of the obstacle density.

1 Introduction

Living cells are spatially organized, e.g. eukaryotic cells have a confined nucleus containing the DNA and reaction complexes are often bound to the cell membrane. To simulate reaction networks accurately it is therefore important to incorporate the molecules' movement into the models and account for the time it takes for a signal to transmit e.g. from the nucleus to the membrane.

Molecules move by diffusion through biological media such as the cytoplasm, which is a non-solute medium, where an estimated 40% [50, 71] of the available space is occupied by macromolecules, such as proteins, ribosomes, RNA and the cytoskeleton. The environment is called crowded, meaning that the space is densely packed by molecules but individual species are only present at very low concentrations. Macromolecular crowding is especially important on the cell membrane [30], where attaching actin filaments [55] create barriers, that hinder the displacement of membrane bound molecules [44, 46]. In mitochondria more than 60% of the matrix can be occupied by enzymes and proteins [80]. Moreover, the extracellular space between e.g. brain cells [41] is also considered crowded.

The steric repulsions between molecules in a crowded environment force diffusing molecules to move around obstacles, or “crowders”, this slows down diffusion. New

* lina.meinecke@uci.edu.

techniques such as fluorescence-fluctuation analysis [12] have shown that diffusion is not simply slowed down but that crowding can lead to anomalous diffusion, where the mean square displacement (MSD) of the molecule is no longer linear, but sublinear in time. As the crowder density increases, space is divided into subdomains and becomes inhomogeneous. For this fractal space, the dimension decreases to a non integer and the MSD no longer follows the linear law applicable in integer dimensions [5, 37].

The change of the diffusion rate in a crowded environment is a hydrodynamic effect. The excluded volume effect on the reaction rates is a thermodynamic consequence [34] and can be both impeding and promoting. While diffusion limited reaction rates are decreased due to the slower diffusion, transition state limited reactions and dimerizations are accelerated [17] since intermediate products reside longer in the vicinity of reaction complexes and dimers occupy less volume than two monomers. Hindered diffusion also leads to localized reactions and a heterogeneous distribution of products, which increases intrinsic noise [35].

Scaled particle theory (SPT) has been used to describe the thermodynamic effect on the reaction rates in a crowded environment [31, 34, 69]. Another approach is to perform Brownian dynamics (BD) simulations and fit the reaction rates to the microscopic results, [48, 74]. In [6], Michaelis-Menten reaction dynamics are best fitted by fractal kinetics and the results are verified by microscopic cellular automata (CA) simulations. The fractal kinetics are modified in [71] to a Zipf-Mandelbrot distribution of the reaction rates.

To better understand the effects of excluded volume on both diffusion and reactions, accurate reaction-diffusion simulations in the crowded cell environment are needed. The microscopic approaches mentioned above are computationally very expensive due to the high number of collisions in such a medium. In this paper we present a novel multiscale approach to simulate diffusion of a spherical particle surrounded by inert and inactive crowders of any size and shape. We resolve the microscopic positions and shapes of the crowders initially to precompute jump rates for the moving molecules. The molecule follows a random walk on a coarse Cartesian grid that no longer resolves the multiple crowders for computationally more efficient simulations. With our approach we can connect a given distribution of obstacles to a space dependent diffusion map which can be used to compute space dependent reaction rates representing reactions in the crowded environment. The method can easily be extended to moving crowders and an advantage over other techniques such as SPT is the versatility in the shape of the crowders. The upscaling to a coarse grid makes the stochastic simulations computationally much more efficient than BD and CA simulations.

In the next section we present existing models of spatial simulations in systems biology and how they incorporate crowding effects. We then present how the microscopic motion of a molecule can be used to calculate its first exit time (FET) from domains, which provides the jump rates in a coarse grained discrete jump process on the mesoscopic level. We continue by extending the FET approach to include macromolecular crowders. In Section 3.2, we use the jump coefficients and compute a space dependent diffusion map for the macroscopic level and show in Section 3.3 how that affects the reaction rates in the crowded environment. We conclude with numerical experiments in the final section.

Vectors and matrices are written in boldface. A vector $\mathbf{u}$ has the components u_i and the elements of a matrix $\mathbf{A}$ are A_{ij} . The derivative of a variable u with respect to time t is written u_t .

2 Spatial modeling in systems biology

In this section we first present existing models of diffusion simulations in systems biology and then describe how they can be adapted to include macromolecular crowding.

2.1 Models of diffusion in dilute media

Molecules undergoing diffusion and reactions inside living cells are often modeled by the reaction-diffusion equations. These are continuous, deterministic partial differential equations (PDEs) describing the time evolution of the concentrations of molecules. For a diffusing molecule the concentration $u(\mathbf{x}, t)$ is described by the diffusion equation

$$u_t(\mathbf{x}, t) = \gamma_0 \Delta u(\mathbf{x}, t), \quad \mathbf{x} \in \Omega \quad (2.1)$$

with diffusion coefficient γ_0 and suitable boundary conditions on Ω . To include reactions corresponding terms are added. This **macroscopic** description is accurate in the limit of large molecule numbers, when stochastic fluctuations are small and the mean value is the quantity of interest. Important molecules such as DNA or transcription factors are, however, only present at very low copy numbers inside living cells. It has been observed in experiments [18, 53, 59, 61, 67, 75] and shown theoretically [26, 54] that stochastic fluctuations play an important role and a discrete stochastic description is more accurate than the deterministic equations.

We distinguish two levels of accuracy of stochastic models. In the **mesoscopic** model the domain Ω is partitioned into N non-overlapping voxels $\mathcal{V}_i$ with nodes $\mathbf{x}_i$ at the center. The state vector $\mathbf{y}(t)$ contains the number of molecules $y_i(t)$ in each voxel $\mathcal{V}_i$ at time t . The voxels are small enough that the molecules can be considered well mixed inside so that reactions can occur between molecules residing in the same voxel. An individual molecule can jump from a voxel $\mathcal{V}_i$ to a neighboring voxel $\mathcal{V}_j$ to model diffusion. The diffusion master equation (DME) describes the time evolution of the probability to be in state $\mathbf{y}$ of a system with only diffusion

$$\frac{\partial p(\mathbf{y}, t)}{\partial t} = \sum_{i=1}^N \sum_{j=1}^N \lambda_{ij} (\mathbf{y} - \boldsymbol{\mu}_{ij}) p(\mathbf{y} - \boldsymbol{\mu}_{ij}, t) - \lambda_{ii}(\mathbf{y}) p(\mathbf{y}, t), \quad (2.2)$$

where λ_{ij} is the jump propensity from $\mathcal{V}_i$ to $\mathcal{V}_j$ and $\lambda_{ii} = \sum_{j=1}^N \lambda_{ij}$ is the total propensity to leave voxel $\mathcal{V}_i$. The transition vector $\boldsymbol{\mu}_{ij}$ is zero except for $\mu_{ij,i} = -1$ and $\mu_{ij,j} = 1$. Let θ_{ij} be the splitting probability, that a jump from $\mathcal{V}_i$ goes to $\mathcal{V}_j$, then

$$\lambda_{ij} = \theta_{ij} \lambda_{ii}. \quad (2.3)$$

By including reaction terms in a similar manner, the DME can be extended to the reaction-diffusion master equation (RDME). In the presence of bimolecular reactions there exists no analytical solution and a numerical solution is impossible due to the high dimension of $\mathbf{y}$. Instead, one samples trajectories of the system with the stochastic simulation algorithm (SSA), first presented by Gillespie [28] for only reactions and improved in [9, 27]. The algorithm was extended to space dependent problems with a Cartesian partitioning of the domain in [15] implemented in [36]. The propensities λ_{ij} are here used to generate random numbers for the time until the next jump. To represent the complicated geometries present in cells the algorithm was extended to curved boundaries in [43] and adapted for unstructured meshes in [19] with software in [14, 40].

In the more accurate **microscopic** model the molecules are tracked along their Brownian trajectories in a continuous space, continuous time Markov process. Brownian dynamics (BD) simulations discretize time and sample the positions of a particle at these discrete time points from a normal distribution. Versions of this method are for example implemented in the software packages Smoldyn [1], ReaDDy [72] and MCell [45]. Another approach is called Green's function reaction dynamics (GFRD) [79, 81], where protective domains are constructed around individual molecules in which they cannot interact with other molecules. This is an event driven algorithm with an asynchronous time step that is chosen such that the probability to exit the protective domain is small. In [77] the algorithm is improved to eGFRD using the exact first exit times from [13, 64] to make it exact and more efficient. The exit times and exit positions from these domains are sampled to propagate the system until molecules are close enough to interact without sampling all the intermediate jumps.

2.2 Include macromolecular crowding

The macroscopic, mesoscopic and microscopic models presented above are designed to simulate diffusion in a dilute medium. The microscopic model automatically incorporates crowding effects since the molecules are modeled as hard spheres with a given volume, but it becomes computationally very expensive in a densely packed space of inactive crowders, because the protective domains around molecules will be small and many short jumps will be simulated before meeting a potential reaction partner.

Cellular automata (CA) have been used in [6, 10, 71, 76] to simulate diffusion in a crowded environment. This is a lattice, or voxel, based microscopic approach, where each site can hold one molecule and crowders are represented as already occupied lattice points. The jump length is here the size of a molecule which also leads to expensive simulations with many short jumps and the shape of the molecules corresponds to the shape of the chosen lattice. The choice of the lattice, moreover, influences the excluded volume effect [32, 57].

In [70] a mesoscopic approach is used where each voxel can hold more than one molecule. After distributing immobile crowders it is decided which voxels are accessible and which are full. The crowders can move in [21, 78] and the jump propensity to an adjacent node is

scaled by the number of available spaces in the target voxel. Macroscopic nonlinear PDEs are then derived in [21] to model diffusion in the crowded cell environment and the results are validated by physical experiments in [22]. This approach is extended in [65] to derive nonlinear diffusion equations modeling more complicated interactions than steric repulsion between the molecules. Similarly, the averaged occupied volume in the whole domain is used in [47] to rescale the jump propensities. These approaches at most take the averaged occupied volume in the target voxel into account and neglect the microscopic positions, the shape of the molecules and the surrounding medium. Hence only an averaged behavior is observed and the MSD is linear like for normal diffusion but with a reduced diffusion constant [66]:

$$\langle \mathbf{x}^2(t) \rangle = (1 - \phi) \gamma_0 t, \quad (2.4)$$

where ϕ is the occupied volume fraction.

In this paper we present a novel multiscale approach to simulate molecular crowding. We will use the microscopic information of the crowders' positions to recalculate the jump propensities on an overlying mesoscopic mesh. Instead of simulating diffusion in the detailed environment, as in BD, we will have to solve many PDEs on small subdomains resolving the microscopic positions of the crowders. This is similar to homogenization techniques used e.g. for flow simulations in porous media, [8, 51]. The crowding molecules can have any shape and this approach is especially useful when the crowded environment is stationary or evolves on a much slower time scale than the diffusing molecule, so that the jump coefficients can be precomputed and used for a long simulation time. This is reasonable since the macromolecules responsible for the majority of occupied volume are ribosomes, microtubules and actin filaments [17], which are large and hence diffuse on a slower time scale than for example transcription factors. Moreover, it was shown in [12] that anomalous behavior is most likely to happen in a stationary environment, since otherwise averaging effects simply reduce the coefficient of normal diffusion. But, it is important to mention that by computing statistics our method can be made efficient also for moving crowders.

3 Upscaling of the crowding effects

We will now present a method of upscaling the detailed information about diffusion in a crowded environment on the microscopic level to the mesoscopic simulation framework and further to the macroscopic description. Moreover, we describe a way of accounting for crowding effects in the reaction dynamics on the mesoscopic and macroscopic levels.

3.1 Microscopic to mesoscopic: first exit times

In this section we will use the methods developed for microscopic simulations of Brownian motion with protective domains [64], to derive the jump propensities λ_{ij} and splitting probabilities θ_{ij} for the mesoscopic model. For simplicity the illustrations are given in dimension $d = 2$ but the method can be extended to $d = 3$ without modification.

3.1.1 First exit times—Let $c(\mathbf{x}, t)$ be the probability distribution that a molecule in Brownian motion is at $\mathbf{x}$ at time t and has not yet exited a domain ω . If $\mathbf{x}_0$ is the starting position of the molecule diffusing with γ_0 , then $c(\mathbf{x}, t)$ fulfills

$$\begin{aligned} c_t(\mathbf{x}, t) &= \gamma_0 \Delta c(\mathbf{x}, t) & \mathbf{x} \in \omega, \\ c(\mathbf{x}, t) &= 0, & \mathbf{x} \in \partial\omega, \\ c(\mathbf{x}, 0) &= \delta_{\mathbf{x}_0}. \end{aligned} \quad (3.1)$$

The homogeneous Dirichlet boundary condition here models that the particle is removed once it hits the boundary. The survival probability of the particle inside ω until time t is then

$$S(t) = \int_{\omega} c(\mathbf{x}, t) d\omega. \quad (3.2)$$

By Gauss' formula the probability density $p_{\omega}(t)$ that the particle leaves ω at t is

$$p_{\omega}(t) = -\frac{\partial S(t)}{\partial t} = -\gamma_0 \int_{\partial\omega} \mathbf{n} \cdot \nabla c(\mathbf{x}, t) ds, \quad (3.3)$$

where $\mathbf{n}$ is the outward normal. The expected time E for the molecule to leave ω for the first time is given by

$$E = \int_0^{\infty} t p_{\omega}(t) dt = \int_0^{\infty} S(t) dt. \quad (3.4)$$

We now use this FET approach to compute the jump propensities λ_{ij} in the space discrete mesoscopic model. We use a Cartesian grid with space discretization h and N nodes $\mathbf{x}_j$ in the domain Ω . The voxels $\mathcal{V}_i$ are here defined by the dual mesh, see Fig. 3.1(b). Since the molecules are considered well mixed inside the voxels, the domain ω that diffusing particles have to leave to be well mixed in the next voxel has to include the centers of the neighboring voxels. On a Cartesian grid we showed in [49] that solving (3.1) on the circle ω_i with center $\mathbf{x}_i$ and radius h (similarly a line of length $2h$ in 1D or a sphere with radius h in 3D) and choosing $\mathbf{x}_0 = \mathbf{x}_i$ gives the correct exit time from node i , see Fig. 3.1(b). Observe that $\omega_i \not\subset \mathcal{V}_i$ and $\omega_i \cap \omega_j \neq \emptyset$ for neighboring nodes i and j . Using (3.2) and (3.4) the expected exit time E_i from $\mathcal{V}_i$ is

$$E_i = \frac{h^2}{2d\gamma_0}, \quad (3.5)$$

see [25]. Since the jump propensity is the inverse of the exit time this agrees with the mesoscopic rate on Cartesian grids

$$\lambda_{ii} = \frac{2d\gamma_0}{h^2} = E_i^{-1}. \quad (3.6)$$

The probability to leave ω_i through a given part of the boundary ω_{ij} at time t is given by the proportion of fluxes

$$\theta_{ij}(t) = \frac{\int_{\partial\omega_{ij}} \mathbf{n} \cdot \nabla c(\mathbf{x}, t) ds}{\int_{\partial\omega_i} \mathbf{n} \cdot \nabla c(\mathbf{x}, t) ds}, \quad (3.7)$$

and we can compute the expected probability to jump to a certain neighboring voxel by

$$\theta_{ij} = \int_0^\infty \theta_{ij}(t) p_{\omega_i}(t) dt = -\gamma_0 \int_0^\infty \int_{\partial\omega_{ij}} \mathbf{n} \cdot \nabla c(\mathbf{x}, t) ds dt. \quad (3.8)$$

Choosing ω_{ij} to be the quarter segment of the boundary closest to $\mathbf{x}$, see the blue line in Fig. 3.1(b), yields the splitting probability $\theta_{ij} = 0.25$ as expected on a Cartesian grid. The method has been extended to a rectangular grid and possible jumps to the diagonal neighbors in [58].

By conditioning on the first step, these time dependent equations can be converted to equations describing directly the expected quantities [68]. The expected exit time for a molecule starting to diffuse in $\mathbf{x}$ from the domain ω_i fulfills the Poisson's equation

$$\begin{aligned} \gamma_0 \Delta E(\mathbf{x}) &= -1, & \mathbf{x} \in \omega_i, \\ E(\mathbf{x}) &= 0, & \mathbf{x} \in \partial\omega_i. \end{aligned} \quad (3.9)$$

Equivalently, the expected splitting probability for this molecule to exit through the boundary ω_{ij} can be computed by the harmonic measure [63, Ch. 7], and fulfills the Laplace equation

$$\begin{aligned} \Delta \theta_{ij}(\mathbf{x}) &= 0, & \mathbf{x} \in \omega, \\ \theta_{ij}(\mathbf{x}) &= 1, & \mathbf{x} \in \partial\omega_{ij}, \\ \theta_{ij}(\mathbf{x}) &= 0, & \mathbf{x} \in \partial\omega_i \setminus \partial\omega_{ij}. \end{aligned} \quad (3.10)$$

We solve equations (3.9) and (3.10) and evaluate them at $\mathbf{x}_i$ instead of solving the time-dependent equations and the integrals above. It is sufficient to solve (3.10) three times for each node since $\sum_{j=1}^4 \theta_{ij} = 1$.

In the following, we will not simply use the circle ω_i to compute the mesoscopic rates, but we will prohibit the molecule from diffusing where the crowders are located.

3.1.2 Include crowding molecules—The crowding molecules are represented as obstacles or holes in the domain ω_i with reflecting boundary conditions. Equations (3.1), (3.9) and (3.10) describe the diffusion of point particles. To account for the volume of the diffusing molecule its radius is added to the excluded volume for the center of mass, see Fig 3.1(a). We depict the crowder as a circle with radius R , but it is important to mention that any shape is possible for the crowding molecules, see Fig. 3.1(c). The shape of the small (as compared to crowders) diffusing molecule is, however, restricted to circles or spheres with radius r .

Solving (3.9) and (3.10) numerically on the perforated domain ω_i means that the crowding molecules have to be resolved by a fine mesh. But, we have divided the global problem into N smaller local subproblems (one protective domain ω_i around each node i). For each subproblem we have to solve 4 PDE's ((3.9) and three equations of type (3.10)). These equations have to be solved only once in a precomputing step which is straight forward parallelizable. This is similar to the approach in [8] where deterministic local equations are solved on media with porous microstructures. The costly stochastic simulations of the spatial SSA are then performed on the coarse mesh with N nodes, that do no longer resolve the individual obstacles. The boundary conditions on the global domain Ω (reflective or absorbing) are implemented by posing these conditions on the secants of the half or quarter circles, which are the protective domains for boundary nodes, see Fig. 3.2(a). In Fig. 3.2(b) we briefly illustrate how the first exit time approach can be further used to compute the jump rates for a Cartesian grid, discretizing a domain Ω with a curved boundary. Here the part of ω_i originating from the circle is imposed with the boundary conditions in (3.9) and (3.10) and the part originating from Ω with the boundary condition valid on Ω , which is usually reflecting or (partially) absorbing. The circle is then divided in the same way as before to compute the splitting probabilities to the neighboring nodes remaining inside Ω .

The simultaneous interpretation of the moving molecules being well-mixed inside the voxels $\mathcal{V}_i$ and jumping from node $\mathbf{x}_i$ to $\mathbf{x}_j$ leads to problems when including crowders. Consider the case where just the center $\mathbf{x}_i$ is blocked, but voxel $\mathcal{V}_i$ is sufficiently empty to be traversed, see Fig. 3.2(c). In this case the jump into voxel $\mathcal{V}_j$ is possible ($\lambda_{ji} > 0$), but the expected time to leave $\mathcal{V}_i$ is infinity and hence the molecules get trapped inside $\mathcal{V}_i$. This does not agree with the microscopic situation, where molecules diffuse around $\mathbf{x}_i$. To avoid this unrealistic trapping, all jump propensities λ_{ji} to voxels whose vertex is isolated are set to zero. In the case when a node $\mathbf{x}_i$ is covered by the excluded volume (not pictured) equations (3.9) and (3.10) cannot be evaluated. Setting all λ_{ji} to zero in this scenario would over estimate the crowding effect considerably, so we constrain the crowder distribution such that $\mathbf{x}_i$ remains inside ω_i .

By using the expected first exit time from ω_i around $\mathbf{x}_i$ to calculate the jump coefficients in a crowded environment it is the crowder distribution inside the whole circle ω_i that affects the coefficients λ_{ij} and θ_{ij} . This differs from other approaches to simulate diffusion in a crowded environment with a discrete space jump process. In [47, 70, 78] it is only the percentage of occupied volume in the target voxel $\mathcal{V}_j$ and in [33] the difference in occupancy between $\mathcal{V}_j$ and the origin $\mathcal{V}_i$ that affect the jump rate $\lambda_{ij} = \theta_{ij}\lambda_{ii}$. In our approach the microscopic positions of all crowding molecules inside ω_i are resolved and influence the jump coefficients. In the case of non-spherical crowding molecules also the orientation is taken into account and long thin molecules with small volume can have a significant effect on λ_{ij} and θ_{ij} , see Fig. 3.3. Note that in contrast to normal diffusion the jump propensities are no longer symmetric, i.e. in general $\lambda_{ij} \neq \lambda_{ji}$ and $\lambda_{ij} \neq \lambda_{im}$ for $j \neq m$.

3.1.3 Statistics on the mesoscopic level—Solving N local problems where complicated geometries have to be resolved, see Fig. 3.1(c) is computationally expensive and will be inefficient if the crowding molecules move and the coefficients λ_{ij} and θ_{ij} have to be recomputed frequently. Since the crowders' exact location is generally unknown we can compute statistics on a reference domain ω_i for given a percentage of occupied volume, a given shape and size of the molecules and h . Instead of solving $NPDE$ s of type (3.9) and $3N$ of type (3.10) at each time step, we can then sample the coefficients λ_{ij} and θ_{ij} from these precomputed distributions. This will be especially applicable for moving crowders, where new coefficients can be drawn from the distributions on the time scale of their diffusion.

3.2 Mesoscopic to macroscopic: a space dependent diffusion map

In this section we derive a macroscopic diffusion equation with a space dependent diffusion coefficient $\gamma(\mathbf{x})$, representing the effect of macromolecular crowding. We approximate the mesoscopic jump process by Fickian diffusion with a constant diffusion coefficient γ_i inside each voxel $\mathcal{V}_i$. The mesoscopic expected exit time E_i from a node $\mathbf{x}_i$ or voxel $\mathcal{V}_i$ is connected via (3.5) to this diffusion coefficient γ_i . So we obtain a modified version of the macroscopic deterministic diffusion equation (2.1)

$$u_t(\mathbf{x}, t) = \nabla \cdot (\gamma(\mathbf{x}) \nabla u(\mathbf{x}, t)), \quad \mathbf{x} \in \Omega, \quad (3.11)$$

where

$$\gamma(\mathbf{x})|_{\mathcal{V}_i} = \gamma_i = \frac{h^2}{2dE_i}. \quad (3.12)$$

For transferring the mesoscopic jump rate to the less detailed macroscopic level we only use λ_{ij} and the random walk becomes symmetric in each voxel, i.e. $\theta_{ij} = \theta_{im} = 0.25$ for $j \neq m$, but the asymmetry between back and forth jumps is preserved, i.e. $\lambda_{ij} \neq \lambda_{ji}$. Alternatively $\gamma(\mathbf{x})$ can be defined on the edges $\mathcal{V}_{ij}$ (see Fig. 3.1(b)) of voxel $\mathcal{V}_j$ by $\gamma_{ij} = h^2/2(\lambda_{ij} + \lambda_{ji})$.

This corresponds to a mesoscopic jump process with symmetry in $\lambda_{ij} = \lambda_{ji}$ and non-symmetric jumps out of a box $\lambda_{ij} \rightarrow \lambda_{im}$ for $j \neq m$.

The anomalous diffusion is here modeled by a space dependent diffusion coefficient. A different description of anomalous diffusion on the macroscopic level are fractional PDE's (FPDE's), which are used to derive a mesoscopic description in [7], where molecules change their internal state, i.e. their diffusion constant, spontaneously in time. This correlates to our model when the crowding macromolecules are moving and the diffusion constant hence also becomes time-dependent: $\gamma(\mathbf{x}, t)$, in [20] we connect statistics from our mesoscopic description to the internal states model in [7] and hence to a FPDE description on the macroscopic level.

In the next section we will use the diffusion map $\gamma(\mathbf{x})$ to derive space dependent reaction rates.

3.3 Reactions

Approaches to correct the reaction rates for crowding effects use either time dependent reaction rates $k(t)$ [6, 71] or static modifications [17, 31, 33]. Similarly to the latter we will use the space dependent diffusion coefficient $\gamma(\mathbf{x})$ from the previous section to compute mesoscopic reaction rates k_i inside each voxel $\mathcal{V}_i$. This static rate becomes time-dependent $k_i(t)$ if we model moving crowders. According to [39] the dilute mesoscopic rate k_0 for bimolecular reactions in a three dimensional cube of volume h^3 is linked to the effective rate k_{CK} by Collins and Kimball [11] by

$$k_0 = k_{CK} / h^3, \quad k_{CK} = \frac{4\pi\sigma\gamma_0 k_r}{4\pi\sigma\gamma_0 + k_r}, \quad (3.13)$$

where k_r is the intrinsic reaction rate and σ the sum of the two reaction radii. In 2D there is no equivalent formula but approximations are derived in [23, 38].

Assuming constant Fickian diffusion inside each voxel as in Sec. 3.2, we can now compute mesoscopic reaction rates k_i for each voxel by inserting the γ_i from (3.12) into (3.13)

$$k(\mathbf{x}) = \frac{1}{h^3} \frac{4\pi\sigma\gamma(\mathbf{x})k_r}{4\pi\sigma\gamma(\mathbf{x}) + k_r} \quad \text{and} \quad k(\mathbf{x})|_{\mathcal{V}_i} = k_i. \quad (3.14)$$

We can now add a space dependent reaction term to the PDE (3.11) using these space dependent reaction rates k_i . To model reactions under excluded volume effects on the mesoscopic level the reactions inside each voxel $\mathcal{V}_i$ have their specific reaction rate k_i .

In this model only bimolecular associations are affected by macromolecular crowding, since the hindered diffusion changes the hitting time for the reaction partners. In the internal states model [7] also birth-death processes and isomerizations become anomalous. It is, however,

questionable if it is meaningful to talk about birth-death processes, when considering excluded volume effects, since all reactants and products also occupy space. With scaled particle theory [30] also dissociation events are affected by the excluded volume which is due to two spherical molecules having a different activity coefficient than one molecule with the same total area. In our model, dissociation is not affected either.

In Section 4.4, we perform numerical experiments to examine for which parameters crowding molecules enhance or decrease the rate of bimolecular reactions.

4 Numerical Experiments

In the following experiments we solve (3.9) and (3.10) in 2D with COMSOL Multiphysics on ω_i , $i = 1 \dots N$. To be able to evaluate the solutions at $\mathbf{x}_i$ the crowders are randomly distributed such that the nodes $\mathbf{x}_i$ remain inside the perforated domain ω_i and are not cut out by the excluded volume.

4.1 Effect of crowding on jump propensities

We first investigate how the jump propensity λ_{ij} changes in different crowding situations. We therefore compute λ_{ij} on a reference domain ω_i with $h = 1$ and different crowders and sizes of the moving molecule r and compare it to the jump rate $\lambda_{0,ij}$ in dilute medium. In Fig. 4.1, we compare the mean value of the jump propensities $\mathbb{E}[\lambda_{ij}]$ for different distributions of crowders and an increasing percentage of occupied volume ϕ with the jump propensities when no crowders are present, where $\mathbb{E}[\lambda_{0,ij}] = \lambda_{0,ij} = 4$. We test two different sizes of crowding molecules for both rectangles and spheres. The reference line is the linear scaling where $\lambda_{ij} = (1 - \phi)\lambda_{0,ij}$ as in [47, 66].

We observe that small obstacles (blue and orange in Fig. 4.1) hinder diffusion more than big crowders for the same percentage of occupied volume, since they have more reflecting surfaces than larger crowders. The same holds for elongated rectangular crowders (green and orange in Fig. 4.1), as they create long barriers without occupying a lot of volume. In three space dimensions the crowding effect is weaker and higher occupation fractions ϕ would be necessary for a similar slow down. Since multiple small spheres or a cylinder of the same size as a large sphere also have larger surface areas in three dimensions, the same relative effects of crowders of different shapes are expected. An increasing size r of the diffusing molecule leads to an increase in the crowding effect, which is intuitive, since a bigger molecule finds less holes through which to escape. These results agree with the findings in [62] and [16]. We see that the averaged linear reduction of the jump propensity can be a good model when the diffusing molecule is about a tenth of the size of the crowders, but over- or underestimates the effect of occupied volume when the diffusing species is smaller or bigger, respectively. Since an average protein has a radius of ca. 2nm [66] and the biggest macromolecules in the cell, the ribosomes, have a radius of up to 15nm the linear correction is a good approximation for many scenarios. The reduction in jump propensity, however, starts to behave exponentially, as in [33], for large diffusing molecules. The case $r = 0$ corresponds to a point particle which is irrelevant when simulating excluded volume effects, but we include it to show the limit for very small particles. To confirm these mesoscopic jump rates we compare them to the inverse of the expected exit time computed by a

Brownian dynamics simulation. We simulate 10^4 trajectories with the open source software Smoldyn [1, 2] for 10 different crowder distributions and equally sized crowding and moving molecules with $R = r = 0.1$ and see in Fig. 4.1(e) that the computationally expensive microscopic results agree well with the mesoscopic coefficients. In our previous work [57] we have compared the computational time for detailed Brownian dynamics simulations on the full domain Ω with microscopic grid based methods and measured a 42-fold speedup. Coarser mesoscopic simulations on Ω will be even faster than the CA simulations and our method hence promises a great save in computational time compared to detailed BD simulations.

In Fig. 4.2, the standard deviation $\sigma(\lambda_{ij}/\lambda_{0,ij})$ initially increases as more and more crowders are added but converges towards zero when the system approaches the state where no escape to the boundary is possible.

Simply rescaling the jump propensity λ_{ij} for each node i by a constant factor will lead to normal diffusion at reduced rate. To observe anomalous diffusion in the crowded environment it is helpful to investigate the mean square displacement (MSD).

4.2 The mean square displacement

As mentioned in Section 2.2 the MSD is linear in time for normal diffusion

$$\langle \mathbf{x}^2(t) \rangle = 2d\gamma_0 t, \quad (4.1)$$

but for anomalous diffusion the relation is no longer linear

$$\langle \mathbf{x}^2(t) \rangle = 2d\gamma_0 t^\alpha, \quad (4.2)$$

where $\alpha < 1$ for subdiffusion. In [12, 24, 60] it was shown that diffusion in a crowded environment can be modeled by a temporal change of the diffusion constant. First the molecule diffuses normally with rate γ_0 for very short time-scales, before it undergoes a transient anomalous phase with a changing diffusion coefficient γ and finally stagnates into normal diffusion at a lower diffusion rate γ_∞ . The initial normal diffusion represents the time the molecule diffuses in the solution before it encounters the first adjacent macromolecule and is slowed down by collisions. On a large time scale the molecule appears to diffuse in a denser medium instead of around obstacles, hence the reduced diffusion rate γ_∞ , see Fig. 4.3. If the crowding macromolecules are distributed evenly the MSD decays monotonically between γ_0 and γ_∞ (pale line), but due to stochastic variations in the medium it fluctuates before converging to γ_∞ (dark line). In Fig. 4.3(a) we only depict collisions with the macromolecules responsible for excluded volume effects, but note that there are many collisions with the much smaller solvent molecules responsible for the Brownian motion.

Since we choose $h > R$ a jump in the mesoscopic model spans a number of macromolecules and the initial free diffusion phase is not resolved and we start to observe diffusion after the first jump of length h , that occurs after a critical time t_c which can be approximated by

$$t_c \sim \frac{h^2}{2d\gamma_0}. \quad (4.3)$$

In the following we will plot the $\langle \mathbf{x}^2 \rangle / 2d\gamma_0 t$ in log-log-scale for different crowding situations to examine when anomalous behavior occurs. Let $\mathbf{p}(t) \in \mathbb{R}^N$ be the probability vector for a diffusing molecule, such that $p_i(t)$ is the probability that the molecule is in voxel $\mathcal{V}_i$ at time t . As described in Section 2, $\mathbf{p}(t)$ evolves by the master equation

$$\dot{\mathbf{p}} = \mathbf{D}\mathbf{p}(t), \quad \mathbf{p}(0) = \mathbf{p}_0, \quad (4.4)$$

where $D_{ij} = \lambda_{ji}$ for $i \neq j$ and $D_{ii} = -\lambda_{ii}$. The initial probability distribution $\mathbf{p}_0$ is $(0, \dots, 1, \dots, 0)^T$ with one at the starting node $\mathbf{x}_0$. We choose the discretization such that $\mathbf{D}$ is small enough to solve (4.4) numerically and compute the mean square displacement by

$$\langle (\mathbf{x}(t) - \mathbf{x}_0)^2 \rangle = \sum_{i=1}^N p_i(t) (\mathbf{x}_i - \mathbf{x}_0)^2. \quad (4.5)$$

In the following experiments we discretize the square $[0, 1] \times [0, 1]$ into $N = n^2$ voxels with space discretization $h = 1/(n - 1)$. If not mentioned otherwise we release the molecules in $[0.5, 0.5]$ at time $t = 0$ and choose $n = 41$. To avoid boundary effects we set homogeneous Dirichlet boundary conditions on Ω and show the solutions as long as more than 99% of the mass is preserved, i.e. $\sum_{i=1}^N p_i(t) > 0.99$.

4.2.1 The effect of γ_0 and ϕ —In Fig. 4.4(a) we plot $MSD(4\gamma_0 t)$ in the crowded environment for different distributions of crowders. Lines in the same color show diffusion in the same environment with starting positions $[0.5, 0.5]$ (solid) and $[0.5 \pm h, 0.5 \pm h]$ (dashed). We clearly observe the anomalous behavior since $MSD(4\gamma_0 t)$ is not constant in time and the fluctuations due to the variations of the local environment around the starting position, but for longer times they converge towards the same long time behavior, before the boundary effects become apparent.

We choose the distributions and starting positions of the curves highlighted in grey to examine the effect of γ_0 and ϕ on the MSD. In Fig. 4.4(b) we observe that the diffusion constant γ_0 only affects when the molecule undergoes anomalous diffusion but the length of the anomalous phase and the long time behavior are independent of γ_0 . The percentage of occupied volume ϕ on the other hand changes both, the average diffusion constant in the

long time behavior and the duration of the transient regime of anomalous diffusion, Fig 4.4(c).

4.2.2 Dependence on the space discretization h —The mesoscopic model is designed for a voxel size h considerably larger than the molecular radius in order to save computational effort compared to a microscopic simulation. For $h \rightarrow 0$ the dilute and well-mixed assumptions in each voxel do no longer hold and the mesoscopic model is known to break down for the simulation of bimolecular reactions [42]. Different corrections to the reaction rates have been suggested [29] and the references therein, but a minimal $h_{min} > R$ remains and space cannot be resolved any finer in the mesoscopic model. For a finer resolution one has to switch to microscopic models, such as BD or CA and we examine the effect of h only for $h \gg R$. A larger h shifts the critical time t_c after which we start to observe the molecule's motion to the right in Fig. 4.3(b), so for very large h we will only see the long time behavior. In Fig. 4.4(d) we see that the initial faster diffusion with $\gamma \sim \gamma_0$ is less resolved for large h where the trajectories start at a much later time. Furthermore the boundary effects become apparent earlier for a larger h , but all discretizations are expected to converge towards the same long time behavior.

4.3 Comparison of mesoscopic and macroscopic simulations

The MSD is only one quantity of interest to examine, but since it is a mean not all features are captured and we will now compare the distributions of molecules resulting from either a mesoscopic or macroscopic simulation. Again, we discretize the square $[0, 1] \times [0, 1]$ with homogeneous Dirichlet boundary conditions into 41 nodes in each direction and let molecules start diffusing in $(0.5, 0.5)$ in an environment with rectangular crowders of different sizes. We solve (4.4) once with the mesoscopic $\mathbf{D}$ and once with $\tilde{\mathbf{D}}$, where the off-diagonal elements are all equal to $\lambda_{ii}/4$, corresponding to a finite difference approximation of the macroscopic equation with the space dependent diffusion constant $\gamma(\mathbf{x})$ derived from the λ_{ii} 's. In Fig. 4.5 the macroscopic model agrees with the mesoscopic results for small and evenly distributed crowding molecules, whereas for long barriers only the mesoscopic approach simulates the expected behavior. This is due to the symmetrization of $\tilde{\mathbf{D}}$, so that only $\mathbf{D}$ can capture the asymmetric diffusion close to the barriers. The diagonal barriers are not completely impermeable in the mesoscopic model since a small part of the boundary ω_{ij} remains.

4.4 Reaction rates

Due to the reduction of diffusion in a crowded environment and (3.14) the overall reaction rate is decreased. It has, however, been shown [30, 71], that protein associations can also be enhanced. We examine the mean time τ_j until the bimolecular reaction

happens, where reactant A is confined to voxel $\mathcal{V}_i$ and molecule B starts diffusing in voxel $\mathcal{V}_j$ at time $t = 0$, see Fig. 4.6(a). Due to molecular crowding we assume a simplified space

dependent diffusion map with $\gamma_i < \gamma_0$ inside $\mathcal{V}_i$ and $\gamma < \gamma_0$ in the rest of the domain. With k_i given by (3.14) and λ_{ii} by (3.6) we can use conditioning on the first step to compute the expected time until the reaction happens:

$$r_i = \frac{k_i}{k_i + \lambda_{ii}} \frac{1}{k_i + \lambda_{ii}} + \frac{\lambda_{ii}}{k_i + \lambda_{ii}} \left[\frac{1}{k_i + \lambda_{ii}} + \sum_m \theta_{im} E(\mathbf{x}_m) + r_i \right] \quad (4.7)$$

$$r_j = E(\mathbf{x}_j) + \frac{h^2 + 4\gamma_i \sum_m \theta_{im} E(\mathbf{x}_m)}{h^2 k_i}, \quad (4.8)$$

where $E(\mathbf{x}_m)$ is the expected time it takes a molecule located in the neighboring voxel $\mathcal{V}_m$ to jump into voxel $\mathcal{V}_i$ and can be computed by solving

$$\mathbf{p}_t(t) = (\mathbf{D} - \mathbf{K}_i) \mathbf{p}(t), \quad \mathbf{p}(0) = \mathbf{p}_0, \quad (4.9)$$

$$E(\mathbf{x}_m) = \int_0^\infty \sum_{k=1}^N |\mathcal{V}_k| p_k(t) dt, \quad (4.10)$$

where $\mathbf{K}_i$ models a sink at node $\mathbf{x}_i$ and is the zero matrix except for a suitably large K_{ii} (e.g. $K_{ii} = 10^9$) and $\mathbf{p}_0$ is the zero vector except for $p_{0,m} = 1/h^3$, see [56] for a derivation. We solve these equations numerically in 3D for a cube with length $L = 1$ and a uniform discretization with $h = 0.1$ in space and reflecting boundary conditions. The voxel $\mathcal{V}_i$ where the reaction happens is chosen to be the center voxel, such that $E(\mathbf{x}_m)$ are equal for all 6 neighbors. The diffusing molecule B starts in $\mathbf{x}_j = (0.7, 0.5, 0.5)$. In Fig. 4.6 we compare the mean binding time in the crowded $\mathbf{E}_j^r$ environment with different γ_i and γ to the time $\mathbf{E}_{j,0}^r$ it takes to react in a dilute solution where $\gamma(\mathbf{x}) = \gamma_0 = 1$. The data points with scaled error bars ($\pm (\frac{\sigma}{\sqrt{M_j^r}} + \frac{\sigma_0}{\sqrt{M_{j,0}^r}})$) are from a SSA simulation of the reaction-diffusion process with $M = 200$ trajectories for $k_r = 10^{-4}$ and $k_r = 10^{-3}$ and $M = 500$ for $k_r = 5 \times 10^{-3}$ and $k_r = 10^{-2}$.

An overall slower diffusion rate $\gamma < \gamma_0$ as a result of obstacles reduces the rate of bimolecular reactions (3.14) in each voxel. But, due to an uneven distribution of crowding agents compartmentalization with locally differing diffusion rates can occur inside the cells. In this case Fig. 4.6 shows that our model of reaction-diffusion dynamics in a crowded environment can model the increase of reaction rates due to crowders. For certain intrinsic reaction parameters the overall reaction rate increases for a compartmentalization where γ_i is smaller than γ , despite the locally slower reaction. The intuitive explanation for this is that once the diffusing molecule enters voxel $\mathcal{V}_i$ it escapes slower and hence gets trapped close to its reaction partner, which increases the chance of collisions. Like this, cells can boost their efficiency by locating important reaction complexes in areas of slower diffusion, which

will be especially productive for reaction cascades where intermediate products are already produced inside the compartment and have a low chance of escaping before being processed further. The fact that macromolecular crowding and locally slower diffusion rates can change the qualitative behavior of a multistep reaction have also been shown by microscopic simulations [77] and experimentally [3]. In the limit when $\gamma_i \rightarrow 0$ the binding time goes towards infinity, since then both reactants are immobile inside $\mathcal{V}_i$ and never collide. For the case $\gamma_i = 1$ the reaction dynamics inside voxel i behave as in the dilute case with $\gamma_0 = 1$ and the time until reaction is hence only governed by the expected time to reach voxel i , which is inversely proportional to the diffusion rates γ and independent of k_r .

5 Conclusion

We have presented a multiscale framework to model diffusion and reactions in a crowded environment, which is an important feature for realistic simulations inside living cells and on their membranes. First, we homogenize the system by solving a set of PDEs on local domains resolving the microscopic positions and shapes of the crowding molecules. This precomputing step is perfectly parallelizable and yields local first exit times, which can be transformed into the jump rates on an overlying Cartesian grid at the mesoscopic level. We then use these local first exit times to compute a space dependent diffusion coefficient for the macroscopic diffusion equation, which corresponds to space dependent reaction rates according to the formula by Collins and Kimball.

Our approach is general in the sense that the crowding molecules can have arbitrary shapes and can be located anywhere inside the domain. We indicate how to adapt our method to moving crowders by computing statistics which is presented in more detail in [20]. As the jump process is simulated on a coarse Cartesian mesh, no longer resolving the numerous crowders, the stochastic simulation is computationally much more efficient than a microscopic simulation capturing all the collisions.

In numerical experiments we foremost observe that shape and size considerably affect how strongly diffusion is impeded: small crowders have more reflective surface and hence hinder diffusion more severely than bigger obstacles, so do elongated crowders, which create long barriers. The effect is also stronger for larger diffusing molecules than for smaller ones, since the former need bigger gaps to pass through. This gives some new insight into how non-idealized (non-spherical) macromolecules affect the diffusion, since most existing models either assume that all particles are spheres or only consider the percentage of occupied volume.

Comparing the mesoscopic and macroscopic models for diffusion in the crowded environment we note that the former captures the asymmetries created by long barriers better and that they both behave similarly for small crowding molecules compared to the grid size.

The space dependent diffusion rate can be interpreted as a compartmentalization effect, which has been observed in cells. In a simplified example we see that reactions located inside a compartment with high crowding/low diffusivity can be enhanced since the reaction

partners reside longer in the vicinity of each other. Hence, the concentration of reaction complexes in an area with slow diffusion as compared to the rest of the cytoplasm or cell membrane can increase the reaction turn-over, an effect that has been capitalized by cells through colocalization of reaction complexes and scaffolding. Otherwise, reactions between initially distant molecules are impeded by excluded volume since it takes longer time for the reactants to find each other.

Hard sphere reflections on obstacles are not the sole cause of anomalous diffusion [69], but there are other interactions between macromolecules, such as transient binding or electrostatic repulsion, which have been modeled by a continuous time random walk [4, 73] and fractional or multifractional Brownian motion [52]. We can include these types of interactions, by modifying boundary conditions on the crowders from reflecting to partially absorbing or adding potential barriers.

Acknowledgments

This work was supported by the Swedish Research Council grant 621-2001-3148 and the NIH grant for StochSS with number 1R01EB014877-01. The author would like to thank the Computational Systems Biology group at Uppsala University for fruitful discussions and Markus Eriksson for the Smoldyn simulations.

References

1. Andrews SS, Addy NJ, Brent R, Arkin AP. Detailed simulations of cell biology with Smoldyn 2.1. *PLoS Comput Biol*. 2010; 6(3):1209–1213.
2. Andrews SS, Bray D. Stochastic simulation of chemical reactions with spatial resolution and single molecule detail. *Phys Biol*. 2004; 1(3–4):137–151. [PubMed: 16204833]
3. Aoki K, Yamada M, Kunida K, Yasuda S, Matsuda M. Processive phosphorylation of ERK MAP kinase in mammalian cells. *Proc Natl Acad Sci U S A*. 2011; 108:12675–12680. [PubMed: 21768338]
4. Barkai E, Garini Y, Metzler R. Strange kinetics of single molecules in living cells. *Phys Today*. 2012; 65(8):29–35.
5. Ben-Avraham, D., Havlin, S. Diffusion and reactions in fractals and disordered systems. Cambridge University Press; 2000.
6. Berry H. Monte Carlo simulations of enzyme reactions in two dimensions: fractal kinetics and spatial segregation. *Biophys J*. 2002; 83(4):1891–1901. [PubMed: 12324410]
7. Blanc E, Engblom S, Hellander A, Lötstedt P. Mesoscopic Modeling of Stochastic Reaction-Diffusion Kinetics in the Subdiffusive Regime. *Multiscale Model Simul*. 2016; 14(2):668–707. [PubMed: 29046618]
8. Brown DL, Peterseim D. A Multiscale Method for Porous Microstructures. Nov.2014 ArXiv e-prints.
9. Cao Y, Gillespie DT, Petzold LR. The slow-scale stochastic simulation algorithm. *J Chem Phys*. 2005; 122:014116.
10. Cianci C, Smith S, Grima R. Molecular finite-size effects in stochastic models of equilibrium chemical systems. *J Chem Phys*. 2016; 084101(144):1–35.
11. Collins FC, Kimball GE. Diffusion-controlled reaction rates. *J Colloid Sci*. 1949; 4:425–437.
12. Di Rienzo C, Piazza V, Gratton E, Beltram F, Cardarelli F. Probing short-range protein Brownian motion in the cytoplasm of living cells. *Nat Commun*. 2014; 5:5891. [PubMed: 25532887]
13. Donev A, Bulatov VV, Oppelstrup T, Gilmer GH, Sadigh B, Kalos MH. A first-passage kinetic Monte Carlo algorithm for complex diffusion-reaction systems. *J Comput Phys*. 2010; 229:3214–3236.

14. Drawert B, Engblom S, Hellander A. URDM: a modular framework for stochastic simulation of reaction-transport processes in complex geometries. *BMC Syst Biol.* 2012; 6:76. [PubMed: 22727185]
15. Elf J, Ehrenberg M. Spontaneous separation of bi-stable biochemical systems into spatial domains of opposite phases. *Syst Biol.* 2004; 1:230–236.
16. Ellery AJ, Baker RE, Simpson MJ. Calculating the Fickian diffusivity for a lattice-based random walk with agents and obstacles of different shapes and sizes. *Phys Biol.* 2015; 12(6):066010. [PubMed: 26599468]
17. Ellis RJ. Macromolecular crowding: An important but neglected aspect of the intracellular environment. *Curr Opin Struct Biol.* 2001; 11(1):114–119. [PubMed: 11179900]
18. Elowitz MB, Levine AJ, Siggia ED, Swain PS. Stochastic gene expression in a single cell. *Science.* 2002; 297:1183–1186. [PubMed: 12183631]
19. Engblom S, Ferm L, Hellander A, Lötstedt P. Simulation of stochastic reaction-diffusion processes on unstructured meshes. *SIAM J Sci Comput.* 2009; 31:1774–1797.
20. Engblom S, Lötstedt P, Meinecke L. Mesoscopic modeling of random walk and reactions in crowded media. 2017 to appear.
21. Fanelli D, McKane AJ. Diffusion in a crowded environment. *Phys Rev E - Stat Nonlinear, Soft Matter Phys.* 2010; 82(2):1–4.
22. Fanelli D, McKane AJ, Pompili G, Tiribilli B, Vassalli M, Biancalani T. Diffusion of two molecular species in a crowded environment: theory and experiments. *Phys Biol.* 2013; 10(4):045008. [PubMed: 23912053]
23. Fange D, Berg OG, Sjöberg P, Elf J. Stochastic reaction-diffusion kinetics in the microscopic limit. *Proc Natl Acad Sci U S A.* Nov; 2010 107(46):19820–5. [PubMed: 21041672]
24. Galanti M, Fanelli D, Maritan A, Piazza F. Diffusion of tagged particles in a crowded medium. *EPL (Europhysics Lett.)* 2014; 107(2):20006.
25. Gardiner, CW. Springer Series in Synergetics. 3. Springer-Verlag; Berlin: 2004. Handbook of Stochastic Methods.
26. Gardiner CW, McNeil KJ, Walls DF, Matheson IS. Correlations in stochastic theories of chemical reactions. *J Stat Phys.* 1976; 14(4):307–331.
27. Gibson MA, Bruck J. Efficient exact stochastic simulation of chemical systems with many species and many channels. *J Phys Chem.* 2000; 104(9):1876–1889.
28. Gillespie DT. A general method for numerically simulating the stochastic time evolution of coupled chemical reactions. *J Comput Phys.* 1976; 22(4):403–434.
29. Gillespie DT, Hellander A, Petzold LR. Perspective: Stochastic algorithms for chemical kinetics. *J Chem Phys.* 2013; 138(17)
30. Grasberger B, Minton C, DeLisi AP, Metzger H. Interaction between proteins localized in membranes. *Proc Natl Acad Sci U S A.* 1986; 83(17):6258–6262. [PubMed: 3018721]
31. Grima R. Intrinsic biochemical noise in crowded intracellular conditions. *J Chem Phys.* 2010; 132(18)
32. Grima R, Schnell S. A systematic investigation of the rate laws valid in intracellular environments. *Biophys Chem.* 2006; 124(1):1–10. [PubMed: 16781049]
33. Grima R, Schnell S. A mesoscopic simulation approach for modeling intracellular reactions. *J Stat Phys.* 2007; 128(1–2):139–164.
34. Hall D, Minton AP. Macromolecular crowding: Qualitative and semiquantitative successes, quantitative challenges. *Biochim Biophys Acta - Proteins Proteomics.* 2003; 1649(2):127–139.
35. Hansen MMK, Meijer LHH, Spruijt E, Maas RJM, Rosquelles MV, Groen J, Heus HA, Huck WTS. Macromolecular crowding creates heterogeneous environments of gene expression in picolitre droplets. *Nat Nanotechnol.* 2015; 11(October):1–8.
36. Hattne J, Fange D, Elf J. Stochastic reaction-diffusion simulation with MesoRD. *Bioinformatics.* 2005; 21:2923–2924. [PubMed: 15817692]
37. Havlin S, Ben-Avraham D. Diffusion in disordered media. *Adv Phys.* 2002; 51(1):187–292.
38. Hellander S, Hellander A, Petzold L. Reaction-diffusion master equation in the microscopic limit. *Phys Rev E - Stat Nonlinear, Soft Matter Phys.* 2012; 85(4):1–5.

39. Hellander S, Hellander A, Petzold L. Reaction rates for mesoscopic reaction-diffusion kinetics. *Phys Rev E*. 2015; 91(2)
40. Hepburn I, Chen W, Wils S, De Schutter E. STEPS: efficient simulation of stochastic reaction-diffusion models in realistic morphologies. *BMC Syst Biol*. 2012; 6:36. [PubMed: 22574658]
41. Hrabe J, Hrabětová S, Segeth K. A model of effective diffusion and tortuosity in the extracellular space of the brain. *Biophys J*. 2004; 87(3):1606–1617. [PubMed: 15345540]
42. Isaacson SA. The reaction-diffusion master equation as an asymptotic approximation of diffusion to a small target. *SIAM Journal on Applied Mathematics*. 2009; 70(1):77–111.
43. Isaacson SA, Peskin CS. Incorporating diffusion in complex geometries into stochastic chemical kinetics simulations. *SIAM J Sci Comput*. 2006; 28(1):47–74.
44. Jin S, Verkman AS. Single particle tracking of complex diffusion in membranes: Simulation and detection of barrier, raft, and interaction phenomena. *J Phys Chem B*. 2007; 111(14):3625–3632. [PubMed: 17388520]
45. Kerr RA, Bartol TM, Kaminsky B, Dittrich M, Chang JCJ, Baden SB, Sejnowski TJ, Stiles JR. Fast Monte Carlo simulation methods for biological reaction-diffusion systems in solution and on surfaces. *SIAM J Sci Comput*. 2008; 30(6):3126–3149. [PubMed: 20151023]
46. Krapf, D. *Mechanisms Underlying Anomalous Diffusion in the Plasma Membrane*. Vol. 75. Elsevier Ltd; 2015.
47. Landman KA, Fernando AE. Myopic random walkers and exclusion processes: Single and multispecies. *Phys A Stat Mech its Appl*. 2011; 390(21–22):3742–3753.
48. Lee B, LeDuc PR, Schwartz R. Stochastic off-lattice modeling of molecular self-assembly in crowded environments by Greens function reaction dynamics. *Phys Rev E*. 2008; 78(3):031911.
49. Lötstedt P, Meinecke L. Simulation of stochastic diffusion via first exit times. *J Comput Phys*. Nov. 2015 300:862–886. [PubMed: 26600600]
50. Luby-Phelps K. Cytoarchitecture and physical properties of cytoplasm: volume, viscosity, diffusion, intracellular surface area. *Int Rev Cytol*. 2000; 192:189–221. [PubMed: 10553280]
51. Målqvist A, Peterseim D. Localization of elliptic multiscale problems. *Math Comput*. 2014; 83(290):2583–2603.
52. Marquez-Lago TT, Leier A, Burrage K. Anomalous diffusion and multifractional Brownian motion: simulating molecular crowding and physical obstacles in systems biology. *IET Syst Biol*. 2012; 6(4):134. [PubMed: 23039694]
53. McAdams HH, Arkin A. Stochastic mechanisms in gene expression. *Proc Natl Acad Sci USA*. 1997; 94:814–819. [PubMed: 9023339]
54. McQuarrie DA. Stochastic approach to chemical kinetics. *J Appl Prob*. 1967; 4:413–478.
55. Medalia O, Weber I, Frangakis AS, Nicastro D, Gerisch W, Baumeister G. Macromolecular architecture in eukaryotic cells visualized by cryoelectron tomography. *Science*. 2002; 298(2002):1209–1213. [PubMed: 12424373]
56. Meinecke L, Engblom S, Hellander A, Lötstedt P. Analysis and design of jump coefficients in discrete stochastic diffusion models. *SIAM J Sci Comput*. 2016; 38(1):A55–A83. [PubMed: 28611531]
57. Meinecke L, Eriksson M. Excluded volume effects in on- and off-lattice reaction-diffusion models. *IET Systems Biology*. 2016
58. Meinecke L, Lötstedt P. Stochastic diffusion processes on Cartesian meshes. *J Comput Appl Math*. Mar.2016 294:1–11. [PubMed: 26594087]
59. Metzler R. The future is noisy: The role of spatial fluctuations in genetic switching. *Phys Rev Lett*. 2001; 87:068103. [PubMed: 11497866]
60. Mommer MS, Lebiedz D. Modeling subdiffusion using reaction diffusion systems. *SIAM Journal on Applied Mathematics*. 2009; 70(1):112–132.
61. Munsky B, Neuert G, van Oudenaarden A. Using gene expression noise to understand gene regulation. *Science*. 2012; 336(6078):183–187. [PubMed: 22499939]
62. Muramatsu N, Minton AP. Tracer diffusion of globular proteins in concentrated protein solutions. *Proc Natl Acad Sci U S A*. 1988; 85(9):2984–2988. [PubMed: 3129721]
63. Øksendal, B. *Stochastic Differential Equations*. 6. Springer; Berlin: 2003.

64. Oppelstrup T, Bulatov VV, Donev A, Kalos MH, Gilmer GH, Sadigh B. First-passage kinetic Monte Carlo method. *Phys Rev E*. 2009; 80:066701.
65. Penington CJ, Hughes BD, Landman KA. Building macroscale models from microscale probabilistic models: A general probabilistic approach for nonlinear diffusion and multispecies phenomena. *Phys Rev E*. 2011; 84(4):041120.
66. Phillips, R., Kondev, J., Theriot, J. *Physical Biology of the Cell*. Garland Science, Taylor & Francis Group; New York: Nov. 2008
67. Raj A, van Oudenaarden A. Nature, nurture, or chance: Stochastic gene expression and its consequences. *Cell*. 2008; 135(2):216–226. [PubMed: 18957198]
68. Redner, S. *A Guide to First-Passage Processes*. Cambridge University Press; Cambridge: 2001.
69. Ridgway D, Broderick G, Lopez-Campistrous A, Ru'aini M, Winter P, Hamilton M, Boulanger P, Kovalenko A, Ellison MJ. Coarse-grained molecular simulation of diffusion and reaction kinetics in a crowded virtual cytoplasm. *Biophys J*. 2008; 94(10):3748–3759. [PubMed: 18234819]
70. Roberts E, Stone JE, Luthey-Schulten Z. Lattice microbes: High-performance stochastic simulation method for the reaction-diffusion master equation. *J Comput Chem*. 2013; 34(3):245–255. [PubMed: 23007888]
71. Schnell S, Turner TE. Reaction kinetics in intracellular environments with macromolecular crowding: Simulations and rate laws. *Prog Biophys Mol Biol*. 2004; 85(2–3):235–260. [PubMed: 15142746]
72. Schöneberg J, Ullrich A, Noé F. Simulation tools for particle-based reaction-diffusion dynamics in continuous space. *BMC Biophys*. 2014; 7(1):11. [PubMed: 25737778]
73. Schulz JHP, Barkai E, Metzler R. Aging Renewal Theory and Application to Random Walks. *Phys Rev X*. 2014; 4(1):011028.
74. Smith GR, Xie L, Lee B, Schwartz R. Applying Molecular Crowding Models to Simulations of Virus Capsid Assembly In Vitro. *Biophys J*. 2014; 106(1):310–320. [PubMed: 24411263]
75. Swain PS, Elowitz MB, Siggia ED. Intrinsic and extrinsic contributions to stochasticity in gene expression. *Proc Natl Acad Sci USA*. 2002; 99(20):12795–12800. [PubMed: 12237400]
76. Takahashi K, Arjunan SN, Tomita M. Space in systems biology of signaling pathways - Towards intracellular molecular crowding in silico. *FEBS Lett*. 2005; 579(8):1783–1788. [PubMed: 15763552]
77. Takahashi K, Tanase-Nicola S, ten Wolde PR. Spatio-temporal correlations can drastically change the response of a MAPK pathway. *Proc Natl Acad Sci U S A*. 2010; 107(6):2473–2478. [PubMed: 20133748]
78. Taylor PR, Yates CA, Simpson MJ, Baker RE. Reconciling transport models across scales: The role of volume exclusion. *Phys Rev E*. 2015; 92(4):040701.
79. Van Zon JS, ten Wolde PR. Simulating biochemical networks at the particle level and in time and space: Green's function reaction dynamics. *Phys Rev Lett*. 2005; 94(12):1–4.
80. Verkman AS. Solute and macromolecule diffusion in cellular aqueous compartments. *Trends Biochem Sci*. 2002; 27(1):27–33. [PubMed: 11796221]
81. van Zon JS, ten Wolde PR. Green's-function reaction dynamics: A particle-based approach for simulating biochemical networks in time and space. *J Chem Phys*. 2005; 123:234910. [PubMed: 16392952]

Fig. 3.1.

(a) Excluded volume (grey and red) for the center of mass of the diffusing molecule (blue).
 (b) Cartesian mesh and protective domain ω_i without crowding. (c) Solution of (3.9) with the effect of molecular crowding.

Fig. 3.2.

(a) Boundary treatment. (b) Using the first exit time approach to compute Cartesian jump rates on the boundary of a curved domain Ω . (c) Model error when interpreting molecules as well mixed and jumping between nodes simultaneously.

Fig. 3.3. Not only the occupancy ϕ , but also the microscopic positions and orientations of the crowding molecules affect the jump propensities $\lambda_{ij} = \theta_{ij}\lambda_{ii}$. (a) $\theta_{ij} = 0$. (b) $\theta_{ij} > 0.25$.

Fig. 4.1.

The mean value of the mesoscopic jump coefficients in the crowded environment $\mathbb{E}[\lambda_{ij}]$ compared to $\mathbb{E}[\lambda_{0,ij}] = 4$ in dilute media and its dependence on the occupancy ϕ . Averages are taken over $M = 100$ different crowder distributions. The obstacles are either spheres (blue and red) with radius R or rectangles (orange and green) with ratio of width to length equal to 20. The dashed reference line corresponds to equation (2.4) when only the averaged occupied volume in the target voxel is taken into account. The spherical moving molecule has radius r . In (e) we compare the mesoscopic coefficients with the results from a Brownian dynamics simulation, where we generate 10^4 trajectories for 10 different crowder distributions with the software Smoldyn.

Fig. 4.2. Standard deviation $\sigma(\lambda_{ii}/\lambda_{0,ii})$ around the mean value of the change in jump coefficients in (a) and (d) in Fig. 4.1.

Fig. 4.3.

(a) Diffusion in the crowded cell environment: Initial free diffusion with γ_0 (green). After colliding with the first macromolecules the observed diffusion is slowed down and the molecule's diffusion coefficient decays (orange) to the long time behavior of slower diffusion with constant γ_∞ in a dense medium (red). (b) MSD curve for diffusion in a crowded medium (solid line) and as reference normal diffusion (dashed line). The pale line corresponds to an ideal well mixed medium and the dark line to a realistic medium with stochastic fluctuations in the positions of the crowders.

Fig. 4.4.

The MSD on a mesoscopic grid with $h = 0.025$ for different distributions of spherical crowders with $R = 5 \times 10^{-3}$ and a moving molecule with $r = 5 \times 10^{-4}$. (a) Two different crowder distributions (red and blue), where we vary the starting position of diffusion from the center $[0.5, 0.5]$ (solid line) to one voxel to the right/left and up/down $[0.5 \pm h, 0.5 \pm h]$ (dashed lines) to show the sensibility of the MSD plot to the local environment. The crowding coefficient is $\phi = 0.4$ and the diffusion constant is $\gamma_0 = 1$. (b) By varying the diffusion coefficient γ_0 for the two extreme distributions highlighted in grey in (a) we see that the diffusion coefficient only affects when the molecules undergo anomalous diffusion. (c) Changing the crowding percentage ϕ for $\gamma_0 = 1$ for the same two distributions as in (b) affects both the long time reduced diffusion and the duration of the anomalous phase. (d) Varying the space discretization h for the red distribution in (a) for all 5 starting positions. We see that a finer discretization better resolves the transient regime.

Fig. 4.5.

Mesososcopic and macroscopic simulations with crowders of different sizes and a moving molecule with radius $r = 10^{-3}$ starting in the center of the domain (red dot). The heat maps show the probability distribution $\mathbf{p}(0.5)$ of the location of the diffusing molecule at $t = 0.5$, which is the solution to equation (4.4) with homogeneous Dirichlet boundary conditions. (a) Rectangles of size 0.0005×0.01 and $\phi = 0.01$. (b) & (c) The mesoscopic ($\mathbf{D}$) and symmetrized macroscopic ($\tilde{\mathbf{D}}$) simulation results with the distribution in (a), respectively. (d) 5 rectangles of size 0.004×0.8 . (e) & (f) The mesoscopic ($\mathbf{D}$) and symmetrized macroscopic ($\tilde{\mathbf{D}}$) simulation results with the distribution in (d), respectively.

Fig. 4.6.

(a) Two-dimensional projection of the three-dimensional experimental setting where a B molecule (blue) starts diffusing in $\mathbf{x}_j = (0.7, 0.5, 0.5)$ and reacts with A (red) that is confined to voxel V_i with $\mathbf{x}_i = (0.5, 0.5, 0.5)$ (red shaded region). Due to an uneven distribution of crowders we assume that the diffusion rate is γ_i inside V_i and γ (vertical dashed lines in (b) and (c)) in the rest of the domain. In (b) and (c) we compare the time it takes to react in this crowded environment t_j^r to the time it takes in an uncrowded environment $t_{j,0}^r$ with $\gamma_0 = 1$ for different intrinsic reaction rates k_r . (b) $\gamma = 0.7$. (c) $\gamma = 0.9$.