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Metabolic Responses Induced by Compression of Chondrocytes in Variable-Stiffness Microenvironments

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Abstract

Cells sense and respond to mechanical loads in a process called mechanotransduction. These processes are disrupted in the chondrocytes of cartilage during joint disease. A key driver of cellular mechanotransduction is the stiffness of the surrounding matrix. Many cells are surrounded by extracellular matrix that allows for tissue mechanical function. Although prior studies demonstrate that extracellular stiffness is important in cell differentiation, morphology and phenotype, it remains largely unknown how a cell's biological response to cyclical loading varies with changes in surrounding substrate stiffness. Understanding these processes is important for understanding cells that are cyclically loaded during daily in vivo activities (e.g. chondrocytes and walking). This study uses high-performance liquid chromatography - mass spectrometry to identify metabolomic changes in primary chondrocytes under cyclical compression for 0–30 minutes in low- and high- stiffness environments. Metabolomic analysis reveals metabolites and pathways that are sensitive to substrate stiffness, duration of cyclical compression, and a combination of both suggesting changes in extracellular stiffness in vivo alter mechanosensitive signaling. Our results further suggest that cyclical loading minimizes matrix deterioration and increases matrix production in chondrocytes. This study shows the importance of modeling in vivo stiffness with in vitro models to understand cellular mechanotransduction.

Keywords

chondrocyte mechanotransduction; cartilage repair; substrate stiffness; osteoarthritis

Introduction

Mechanotransduction involves the processes by which cells respond to various forms of mechanical loading such as tension, compression, shear, or hydrostatic pressure.

Mechanosensitive pathways are vital for many cellular processes such as metabolism,

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Conflict of Interest Statement

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differentiation, matrix remodeling, and cell survival (Jaalouk and Lammerding, 2009). Cells of structural tissues such as cartilage reside in a dense extracellular matrix that protects the sparse cell population and provides mechanical properties for tissue function. In most tissues, the cells themselves have lower stiffness than their surrounding matrices. Thus, force transmission to the embedded cells is a function of both cell and matrix stiffness (Gao et al., 2014).

Stiffness is a material's resistance to deformation and directly impacts load distribution. Therefore, in two adjacent materials, the one with the lower stiffness will deform more. This explains why cells encapsulated in higher stiffness hydrogels experience larger deformations (Zignego et al., 2014). Cellular force transmission induces conformational changes in the internal structure of the cell, leading to molecular changes that can protect the cells during the dynamic change in environmental conditions (Dowling et al., 2013). Chondrocytes, the lone cell type in cartilage, have an additional matrix called the pericellular matrix (PCM) that forms a thin layer (2–5 μ m) directly surrounding the cell followed by a common ECM found in other tissues (Youn et al., 2006).

Although past work has recognized the importance of cell and surrounding matrix stiffness on cell differentiation, morphology, and phenotype (Engler et al., 2006; Gilbert et al., 2010; Jianping et al., 2010; Zhang et al., 2016), little is known about the metabolomic response to changes in substrate stiffness. In diseases such as osteoarthritis (OA) there is a direct correlation between disease progression and decreases in stiffness of the PCM directly surrounding the chondrocyte (Zhang, 2015). While healthy cartilage has PCM stiffness values of ~40kPa, the stiffness of osteoarthritic PCM is ~24kPa (Alexopoulos et al., 2005). Current studies have analyzed 3D cultures in 1–3% (v/v) agarose hydrogels, which has a stiffness ranging from 15–19kPa (Jutila et al., 2015), falling to the lower boundary for OA PCM environments and providing limited data on the progression of chondrocyte mechanotransduction pathways from healthy to OA. However, recent advances have characterized mechanical properties of higher concentration agarose hydrogels and found that the stiffness of 4.5% (v/v) agarose hydrogels approaches that of healthy PCM. Therefore, comparing 2 and 4.5% agarose hydrogels provide an opportunity for studying altered mechanotransduction in OA disease progression (Jutila et al., 2015).

A PCM stiffness value of 35 kPa represents a region between healthy and OA conditions and could potentially give insight on mechanosensitive changes in the cell at early stages of OA before complete cartilage degradation has occurred. Early detection methods for OA patients are currently limited to MRI joint space reduction and family history (Sinusas, 2012). However, if patients and physicians were able to detect cartilage loss prior to stage IV OA, there could be use of therapeutics through physical therapy sessions. Here we analyze the metabolomic profiles of human OA patient chondrocytes after 0–30 minutes of compression. We find large-scale mechanosensitive changes induced by compression that suggest physical therapy may be a viable option for postponing disease progression or even reversing effects of cartilage matrix deterioration.

The objective of this study is to characterize global differences in cellular behavior at early time points after loading by comparing the metabolomic profiles of cell-encapsulated

hydrogels of varying stiffness. In this study, we applied physiological cyclic compression (1.1Hz, $5\pm 1.9\%$ strain) to 2 and 4.5% (v/v) agarose hydrogels containing primary human chondrocytes for 0, 15 and 30 minutes and quantified the changes in metabolism using high-performance liquid chromatography-mass spectrometry (HPLC-MS) and pathway enrichment analysis (Kamburov et al., 2011; Zhu et al., 2013). We hypothesize that cells in higher stiffness hydrogels will show altered mechanosensitive metabolomic profiles compared to cells in lower-stiffness hydrogels due to increased magnitude in transmitted forces to the cells.

Materials and Methods

Primary human chondrocyte culture and encapsulation

As a model of mechanosensitivity in cells undergoing dynamic loading *in vivo*, primary human chondrocytes from grade IV osteoarthritic hips were obtained from n=5 donors following joint replacement. To isolate chondrocytes, harvested cartilage from each patient was digested overnight in Type IV collagenase (2mg/mL for 12–14 h. at 37°C). Isolated chondrocytes were cultured in DMEM with 10% fetal bovine serum and antibiotics (10,000 I.U./mL penicillin and 10,000 μ g/mL streptomycin) in 5% CO₂ at 37°C. Cells were expanded in monolayer for one passage prior to encapsulation in either 2 or 4.5% (v/v) agarose (Sigma: Type VII-A A0701) using previously established methods (Jutila et al., 2014; Zignego et al., 2015). Chondrocytes were seeded at a concentration of ~500,000 cells/gel (gel diameter=7mm, gel height=12.7mm).

Mechanical Stimulation

To model the *in vivo* mechanical environment of chondrocytes, cells were cyclically compressed in 3D agarose hydrogels. Cell-seeded constructs from each patient (N=5 patients, n=3 samples per patient) were randomly assigned to one of three experiment groups: unloaded controls (0 minutes of loading), 15, or 30 minutes of cyclical compression for both 2% and 4.5% experimental groups. 24 hours after encapsulation, the gels were placed in fresh antibiotic-free Dulbecco's Modified Eagle Medium (DMEM) with 10% fetal bovine serum (FBS) and cyclically compressed using a custom built bioreactor (Jutila et al., 2014). This system provides relatively homogeneous deformations with displacement precision of 1% and strain precision of 6.5% (Zignego et al., 2014). Sinusoidal, compressive strains of $5\pm 1.9\%$ (based on initial $12.7\text{mm} \pm 0.01\text{mm}$ gel height) were applied to the gels at a rate of 1.1 Hz to physiologically mimic the human gait cycle for 0, 15 and 30 minutes (Sutter et al., 2015; Umberger and Martin, 2007). These strains are expected for non-injurious physiological loading. All mechanical testing was performed in physiological cell culture conditions (37°C, 5% CO₂).

Metabolite extraction

To isolate stimulated chondrocytes from agarose hydrogels, cell-seeded constructs were washed twice in phosphate buffered-saline (PBS), immediately flash frozen in liquid nitrogen and pulverized before metabolite extraction in 70:30 methanol:acetone solution. Samples were vortexed every five minutes for the first 20 minutes in solution and held at -20°C overnight for further metabolite extraction. The next day, supernatant was extracted

from samples following centrifugation to remove proteins and remaining agarose gel. Metabolite samples were then placed in a centrifuge under vacuum for 6.5 hours for solvent removal. Remaining dried sample pellets were resuspended in 100 μ L of mass spectrometry grade 95:5 water:acetonitrile solution (Jutila et al., 2014). All reagents were mass-spectrometry grade.

Untargeted metabolic profiling

To identify global changes in cell physiology, we used metabolomic profiling to identify small molecules (metabolites) in control and compressed samples. Extracted metabolites were analyzed using HPLC-MS on an Agilent 6538 quadrupole time-of-flight (QTOF) mass spectrometer in positive mode (resolution: ~20,000ppm, accuracy: ~5ppm, potential adducts: H⁺, Na⁺). Intensity values from m/z values identified in each sample were exported using Agilent MassHunter Qualitative Analysis software. Median intensities of m/z values for each experiment group were calculated and statistically analyzed across groups using a student's t test with false-discovery rate correction. M/z values with a q-value < 0.05 between one or more experimental groups were considered statistically significant. Statistically significant m/z values were clustered into co-regulated metabolites using unsupervised clustering in Matlab and extracted for compound identification in METLIN. KEGG and CAS IDs of identified compounds were imported to IMPaLA to assess pathway enrichment with false discovery rate (FDR) analysis (q < 0.05) (Kamburov et al., 2011; Zhu et al., 2013).

Results

15 minutes of cyclical compression

Prior studies have examined the long term effects of cyclical loading (*e.g.* 1–24 hours) but little research has been reported on short term biological implications (Bian et al., 2010; Davisson et al., 2002; Huang et al., 2010; Mauck et al., 2000; Tsuang et al., 2008). Using a 15-minute time scale allows us to identify the transition of a cell's metabolomic profile from a static to dynamic system (Figure 1A). We confirm changes in metabolomic profiles of samples cyclically compressed for 15 minutes compared to unloaded controls as described below.

Clusters A2 and A7 identify metabolites upregulated in either 2 or 4.5%, respectively (Figure 1A). Cluster A2 contains 126 mass-to-charge (m/z) values that map to 8 statistically significant (Student's t-test, p<0.05, FDR correction) metabolic pathways including: fatty acid and phospholipid metabolisms, and calcium-dependent pathways. Cluster A7 did not identify any pathways from 108 m/z values.

Clusters A3 to A5 identify metabolites upregulated after 15 minutes of loading: A3-metabolites upregulated in 4.5% agarose only, A4-upregulated in both 2 and 4.5% agarose, and A5-upregulated in only 2% agarose. Enrichment of A3 metabolites resulted in 9 significant pathways including: metabolism of alpha-linolenic acid and retinol, adrenaline signaling, platelet aggregation, vitamin A deficiency, and amino acid degradation. Cluster A4 metabolites represent 2 significant pathways including purine and glutamine/glutamate metabolism for both 2 and 4.5%. Cluster A5 contains 0 significant pathways. Cluster A6

represents metabolites downregulated with 15 minutes of loading and includes 2 statistically significant pathways: butanoate and nicotinamate/nicotinamide metabolism.

30 minutes of cyclical compression

The current treatment option for grade IV OA patients consists of complete joint replacement for patients with excessive pain and discomfort during daily tasks (Sinusas, 2012). The rationale for comparing 0 and 30 minutes of compressive loading is to examine a timescale relevant for treatment options over the duration of a typical physical therapy treatment session. Changes in metabolomic profiles were confirmed for 30-minute loading samples compared to unloaded controls and are detailed below.

Cluster B1 shows a downregulation of metabolite intensity in lysine degradation with 30 minutes of loading (Figure 1B). Clusters B5, B6, B7 and B9 identify metabolites upregulated after 30 minutes of loading: (B5) upregulated in 2% agarose only, (B6) upregulated in both 2 and 4.5% agarose, and (B7) and (B9) both identify metabolites upregulated in 4.5% agarose. Cluster B5 contains 50 statistically significant pathways including fatty acid and phospholipid metabolisms. Cluster B6 identifies 10 significant pathways including alpha-linolenic acid, amino acid, and retinol metabolisms, vitamin A deficiency, and glutathione synthesis and recycling. Cluster B7 did not identify any load-related pathways; however cluster B9 contains 7 significant pathways including fructose, mannose, and alpha-linolenic acid metabolisms as well as chondroitin sulfate and dermatan sulfate degradation.

Cluster B3 does not identify any known pathways upregulated only in 4.5% with or without loading. Cluster B4 identifies an upregulation of acyl chain remodeling of cardiolipin in only 2% agarose with and without loading.

Stiffness-Dependent Mechanotransduction

Comparisons of metabolite distributions for 0, 15, and 30 minute time points between 2% and 4.5% agarose show metabolite values distinct to each stiffness group (Figure 2A) and loading conditions (Supplemental Figure 2). Principal Components Analysis (PCA) analysis revealed distinct clustering of all experimental groups with PCA components 1, 2, and 3 representing 30.0%, 8.9% and 7.1% of the total variance, respectively.

Comparing unloaded 2% cell-encapsulated hydrogels with the other 5 experimental groups revealed over 200 m/z values that were detected in unloaded 2% samples that were not detected in all other samples (Figure 2B). In contrast, over 300 m/z values were not detected in unloaded 2% samples that we detected in all other experiment groups revealing both loading- and stiffness-induced changes in metabolomic profiles.

We found significant changes in the distributions of metabolite intensities only when comparing 0 vs 15 minutes and 0 vs 30 minutes in 4.5% agarose hydrogels, not 2% hydrogels (Figure 3). Comparisons between 2% loading groups reveal no significant changes between 0-, 15- and 30-minute time points suggesting that the higher stiffness associated with 4.5% agarose is required for mechanotransduction. These data may also

represent the decreased sensitivity in osteoarthritic chondrocytes to dynamic loading vital for cell survival and extracellular matrix production.

Discussion

After exposing primary human chondrocytes encapsulated in agarose hydrogels to cyclical compression, we observe changes in metabolomic profiles between high- and low-stiffness hydrogels. When comparing 0-, 15- and 30-minute loading groups, data and analyses show that the metabolomic profiles of chondrocytes are substantially altered with as little as 15 minutes of mechanical stimulus (Figure 1A). Using pathway analysis, cellular signaling pathways were uniquely identified varying with time and hydrogel stiffness. The differences in pathway upregulation/downregulation suggest microenvironmental sensitivity to mechanical loading in cell metabolism (Figure 4). Based on prior results, we estimate that the average stresses are at least 40% higher in the 4.5% agarose samples compared with the 2% agarose samples.

Pathways similarly regulated in 2 and 4.5% microenvironments

Upregulated with loading—15 minutes of loading in both 2 and 4.5% agarose hydrogels upregulated purine, glutamine and glutamate metabolism pathways. The result of increased purine metabolism may correspond to known adenosine signaling regulating bone and cartilage health (Strazzulla and Cronstein, 2016). The intracellular and extracellular production of adenosine, a purine nucleoside, acts in response to mechanical stimulation including inflammation. This interaction occurs at the P2-A2A receptor, which has been shown to regulate chondrocyte differentiation and function (Campo et al., 2012). Without tight regulation of extracellular adenosine levels, increases in glycosaminoglycan (GAG) release, matrix metalloproteinase production, prostaglandin E2 and nitric oxide (NO) can induce further inflammation and potentially lead to cell death. Upregulation of glutamine and glutamate metabolism may indicate tricarboxylic acid (TCA) cycle compound alpha-ketoglutarate is being converted to glutamate/glutamine to produce additional building blocks for protein synthesis of matrix molecules. Increased levels of glutamine might also be a cellular survival response to increased nitric oxide production during excess articular chondrocyte activation with loading (Studer et al., 1999). Excess glutamine has been shown to inhibit NO-induced apoptosis in articular chondrocytes (Tonomura et al., 2006).

30 minutes of loading in both 2% and 4.5% agarose upregulated the same pathways as 15 minutes of loading in only 4.5% agarose gels. This suggests a latent mechanosensitive response in low-stiffness microenvironments compared to high-stiffness conditions. These pathways consist of adrenaline signaling, alpha-linolenic acid and retinol metabolism, vitamin A deficiency, and amino acid degradation. Adrenaline signaling through norepinephrine (m/z : 170.0807, adduct: $M+H^+$) previously has been linked to increased apoptosis and the reduction of chondrocyte proliferation in OA cell cultures (Lorenz et al., 2016). Anti-inflammatory and tissue protective effects have been shown in 1:1 to 6:1 ratios of linoleic acid (LA) to alpha-linolenic acid (ALA) inhibiting the decomposition of connective tissue such as type II collagen compared to higher ratios (*e.g.* 10:1) that induce

inflammatory responses (Mengshol et al., 2000; Yu et al., 2015). Further targeted analyses would be required to determine the LA to ALA ratio accurately.

Finally, we see the upregulation of glutathione synthesis and recycling in 30 minutes of loading in both 2 and 4.5% hydrogels only (not unloaded controls) further validating our interpretation of oxidative stress minimization (Watari et al., 2011).

Downregulated with loading—Nicotinamide/nicotinamide metabolism, essential for generating coenzymes nicotinamide adenine dinucleotide (NAD⁺) and nicotinamide adenine dinucleotide phosphate (NADP⁺), used in glycolysis, TCA cycle, pentose phosphate cycle, fatty acid synthesis and other metabolic pathways, showed a statistically significant decrease in intensity after 15 minutes of loading in both 2 and 4.5% hydrogels. Finally the deactivation of lysine degradation upon 30 minutes of dynamic loading in both 2 and 4.5% hydrogels is consistent with mechanically-induced protein/matrix synthesis.

Taken together, these data identify pathways that are sensitive to mechanical compression but independent of substrate stiffness. They further demonstrate that lower-stiffness gels may correspond to delayed mechanosensitive responses leading to imbalances in catabolic and anabolic regulation in cell health leading to further disease progression.

Pathways uniquely regulated in 2 and 4.5% microenvironments

Metabolites found only in 4.5% agarose hydrogels for 0 and 15 minutes of loading (Figure 1A, A7) and 0 and 30 minutes of loading (Figure 1B, B3) fail to identify any statistically significant pathways suggesting large mechanobiological differences between loaded and unloaded controls in higher stiffness microenvironments. In contrast, we find upregulation of fatty acid and phospholipid metabolism throughout all of 2% agarose conditions (Figure 1A, A2 and Figure 1B, B4 and B5) with as many as 50 pathways upregulated in 30 minutes of loading, consistent with increased sensitivity among cells embedded in a lower stiffness matrix leading to increased cell membrane remodeling.

Interestingly, chondroitin and dermatan sulfate, known GAGs in the extracellular matrix of connective tissues, were upregulated in unloaded controls and 30 minutes of cyclical compression in 4.5% hydrogels but were not detected at the 15-minute time point. 30 minutes of cyclical loading in 4.5% agarose hydrogels only resulted in upregulation of several sugar metabolism pathways, consistent with increased GAG production. These pathways were not identified in 2% hydrogel conditions.

Overall, we demonstrate for the first time large-scale changes in chondrocyte mechanotransduction that are dependent on microenvironmental stiffness using metabolomic profiling. These data suggest a link between cartilage matrix deterioration and altered mechanotransduction in OA that could be reversed through therapeutic loading of cartilage (*e.g.* physical therapy).

Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

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Figure 1. Mechanotransduction is regulated by both gel stiffness and mechanical loading

Groupings of metabolites found in (A) 0 and 15 minute loading samples and (B) 0 and 30 minute loading samples from both low-stiffness (2%) and high-stiffness (4.5%) agarose samples using Matlab's heat map hierarchical clustering on the median values. Clusters of interested are outlined and labeled on the right hand side. Cluster A1: On in 2% 0 minute loading only, A2: On in 2% only, A3: On in 4.5% 15 minute loading only, A4: On with 15 minute loading, A5: On 2% 15 minute loading only, A6: Off with loading, A7: On in 4.5% only, A8: On in 4.5% 0 minute loading only. Cluster B1: Off with loading, B2: On with 4.5% 0 minute loading only, B3: On in 4.5% only, B4: On in 2% only, B5: On in 2% 30 minute loading only, B6: On with loading, B7 and B9: On with 4.5% 30 minute loading only, and B8: On in 2% 0 minute loading only.

Figure 2. Both gel stiffness and compression result in large-scale changes in metabolites
 (A) Comparison of metabolite intensity values found in 0-, 15- and 30- minute loading in 2 and 4.5% agarose hydrogels: (Left) comparison of 0-minute loading between 2% (x-axis) and 4.5% (y-axis) metabolite intensity values. 391 statistically significant metabolite intensity values were uniquely identified in 4.5% agarose while 361 were uniquely identified in 2%. (Center) Comparing 15-minute loading groups between 2% (x-axis) and 4.5% (y-axis) agarose found 383 metabolites specific to 4.5% agarose compared to 238 specific to 2%. (Right) Comparing 30 minutes of loading between 2% (x-axis) and 4.5% (y-axis) found 422 metabolites specific to 4.5% agarose compared to 262 specific to 2%. (B) Barplots showing the number of metabolites in each experimental group showing statistically significant upregulation, downregulation and no change compared to 0 minutes of loading in 2% agarose with FDR correction. Blue denoting upregulation, red downregulation and grey as no significant change in intensity. (C) Principal component analysis of 0-, 15-, and 30-minute experimental groups in 2 and 4.5% agarose (Yellow triangle: 0-minute loading in 2% agarose, purple triangle: 15-minute loading in 2%, red triangle: 30-minute loading in 2%, green circle: 0-minute loading in 4.5%, cyan circle: 15-minute loading in 4.5% and dark blue circle: 30-minute loading in 4.5%). Comparisons of principal component 1 (x-axis,

30%) and 2 (y-axis, 8.9%) (Top) and principal components 2 (x-axis, 8.9%) and 3 (y-axis, 7.1%) (Bottom) show clustering of experiment groups with significant overlap of 0-minute loading in 2 and 4.5% agarose.

Figure 3. Mechanical loading changes distributions of metabolites in 4.5% but not 2% agarose
KS analysis comparing metabolite distributions between experimental groups reveal statistically significant ($p \leq 0.05$) changes in metabolomic profiles between 0 and 15 minutes of loading in 4.5% agarose hydrogels (top right) and 0 and 30 minutes of loading in 4.5% agarose hydrogels (middle right). KS analysis of 2% hydrogels (left column) reveal no statistically significant changes in metabolomic profiles with varying loading conditions. Median distributions between 15 and 30 minutes in 4.5% agarose were not significantly different (bottom right).

A

		Agarose Concentration			
		2%		4.5%	
Compression	0 min	UP: Metabolism of Butanoate, Nicotinate & Nicotinamide DOWN: Metabolism of D-glutamine/D-glutamate and Purine			
		UP: Fatty acid/PL metabolism (7), Calcium dependent events DOWN: N/A	UP:Linoleic acid metabolism	UP: Degradation of chondroitin and dermatin sulfate, Sugar metabolism (5)	UP: N/A DOWN: Fatty acid/PL metabolism (7), Calcium dependent events
			UP: N/A	UP: Metabolism of: Retinol, Alpha-linolenic acid, amino acids, Vitamin A deficiency, Adrenaline signaling (4)	
	15 min	UP: Metabolism of D-glutamine/D-glutamate and Purine DOWN: Metabolism of Butanoate, Nicotinate & Nicotinamide			

B

		Agarose Concentration			
		2%		4.5%	
Compression	0 min	UP: Lysine degradation DOWN: Metabolism of: Retinol, Alpha-linolenic acid, amino acids (2), D-glutamine/D-glutamate, and xenobiotics by cytochrome P450, Vitamin C deficiency, Glutathione synthesis and recycling (2)			
		UP: Fatty acid/PL metabolism DOWN: N/A	UP: N/A	UP: Degradation of chondroitin and dermatin sulfate, Sugar metabolism (24), Pentose phosphate pathway	UP: N/A DOWN: Fatty acid/PL metabolism
			UP: Fatty acid/PL metabolism	UP: Degradation of chondroitin and dermatin sulfate, Alpha-linolenic & Sugar metabolism (3),Aromatase inhibitor pathway	
	30 min	UP: Metabolism of: Retinol, Alpha-linolenic acid, amino acids (2), D-glutamine/D-glutamate, and xenobiotics by cytochrome P450, Vitamin C deficiency, Glutathione synthesis and recycling (2) DOWN: Lysine degradation			

Figure 4. Summary of chondrocyte metabolomic pathways sensitive to both substrate stiffness and compressive loading

Metabolomic pathways upregulated and downregulated in 2 and 4.5% agarose comparing (A) 0 vs 15 minutes and (B) 0 vs 30 minutes of compression using Metlin and IMPaLA pathway enrichment results from HPLC-MS analysis. PL: phospholipid.

Table 1

The number of m/z values in each cluster found in Figure 1, the number of candidate metabolites identified using Metlin (15ppm accuracy, possible adducts: H⁺ and Na⁺) and the number of statistically significant pathways identified in IMPaLA using metabolite KEGG and CAS IDs.

Heat Map	Cluster	# M/Z Values	# Candidate Metabolites	# Significant Pathways
0 v 15	A1	116	342	1
	A2	126	389	8
	A3	158	711	9
	A4	517	2048	3
	A5	86	302	0
	A6	70	465	2
	A7	108	712	0
	A8	123	764	9
0 v 30	B1	83	452	1
	B2	171	797	34
	B3	135	1052	0
	B4	99	470	1
	B5	178	965	50
	B6	460	2295	10
	B7	145	645	1
	B8	154	427	1
	B9	204	989	7

Table 2

Pathway analysis associated with 0 vs. 15 minute loading heat map Table lists significant cell metabolism pathways identified in each cluster using IMPaLA enrichment analysis and the metabolites associated with positively identified metabolites in that pathway.

Heat Map	Cluster	Cluster Description	Pathway	Metabolites (KEGG ID)	Metabolites (MetIn)
0 v 15	A1	↑ 2%, 0 min. only	Linoleic acid metabolism	C14829;C14828;C00157	12,13- μ HOMe-(4d); 9,10-dHOME-(4d);PC20;4(5Z,8Z,11Z,14Z)/22;6(4Z,7Z,10Z,13Z,16Z,19Z))
	A2	↑ 2%, ↓ 4.5%	Fatty acid/phospholipid metabolism (7) Calcium dependent events	C04230 C04230	LysophC1(18;3;6Z,9Z,12Z) LysophC1(18;3;6Z,12Z,15Z)
	A3	↑ 4.5%, 15 min. only	Retinol metabolism Vitamin A deficiency Adrenaline signaling (4) Platelet aggregation Alpha-Inolenic acid metabolism Amino acid metabolism	C16677;C11061;C16680;C16679 C16677;C11061;C16680;C16679 C06547;C00788 C06547;C00788 C16346;C16326;C16316;C04780 C15975;C00671;C15979;C00233	all-trans-4-hydroxyretinoic acid; 1-O-all-trans-retinoyl-Beta-glucuronide acid; 5,6-Epoxyretinoic acid; all-trans-; 18-Hydroxyretinoic acid all-trans-4-hydroxyretinoic acid; 1-O-all-trans-retinoyl-Beta-glucuronide acid; 5,6-Epoxyretinoic acid; all-trans-; 18-Hydroxyretinoic acid Noeprinephrine (noradrenalinol); (-)-Epinephrine Noeprinephrine (noradrenalinol); (-)-Epinephrine 17-Hydroxylinolenic acid(9S)-HOTF; 13(S)-HOTF; (9S,13S)-10,11-dihydro-12-oxo-15-phytoenonic acid S-(3-Methylbutanoyl)-dihydroliponamide-E;(S)-3-Methyl-2-oxopentanoic acid; S-(2-Methylbutanoyl)-dihydroliponamide; Kerolactone
	A4	↑ 15 min., ↓ 0 min.	D-Glutamine/D-glutamate metabolism Purine metabolism	C00064;C00819;C02237 C00064;C00862;C05239;C02624;C00201;C02348;C05516;C11821;C01367;C00294;C02350	L-Glutamine; D-Glutamine; (R)-(+)-2-Pyrrolidone-5-carboxylic acid L-Glutamine; deoxyguanosine 5'-monophosphate (dGMP); 5-Aminomidazole-Hyoxanthine; Adenosine monophosphate; (R)-(-)-Alantoin; 5-Amino-4-imidazole carboxylate; 5-Hydroxyisourate; Adenosine 3',5'-
	A5	↑ 2%, 15 min. only	N/A	N/A	N/A
	A6	↑ 0 min., ↓ 15 min.	Butanoate metabolism Nicotinate and nicotinamide metabolism	C01089;C05984;C02727 C02295;C02930;C00922;C15986	D(-)-Beta-hydroxy butyric acid; 2-hydroxy-butanonic acid; Nε-psilon-Acetyl-L-lysine Methylsuccinate; 2-Methylenglutarate; 2,3-Dimethylmalate; 2,6-Dihydroxypseudoxyincotone
	A7	↑ 4.5%, ↓ 2%	N/A	N/A	N/A
	A8	↑ 4.5% 0 min. only	chondroitin sulfate degradation dermatan sulfate degradation Sugar metabolism (5)	C00252;C05403;C00243;C05382;C08240;C08250;C01083;C05402;C00089 C00252;C05403;C00243;C05382;C08240;C08250;C01083;C05402;C00089 C01083;C00243;C00208;C00089;C00252;C08731;C00185;C05400;C01225;C05402;C05403;C05382	Isonalutose; 3'-Ketolactose; D-Lactose; Sedoleptulose 7-phosphate; Gentiolucose; Sophorose; Alpha,Alpha-Trehalose; Melbilucose; Sucrose Isonalutose; 3'-Ketolactose; D-Lactose; Sedoleptulose 7-phosphate; Gentiolucose; Sophorose; Alpha,Alpha-Trehalose; Melbilucose; Sucrose Alpha,Alpha-Trehalose; D-Lactose; Maltose; Sucrose; Isonalutose; 3-Ketolactose; Cellulibiose; Epimelbilucose; Galactinol (1-Alpha-D-galactosyl-myo-inositol); Melbilucose; 3'-Ketolactose; Sedoleptulose 7-phosphate