Video Article

3D Whole-heart Myocardial Tissue Analysis

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Abstract

Cardiac regenerative therapies aim to protect and repair the injured heart in patients with ischemic heart disease. By injecting stem cells or other biologicals that enhance angio- or vasculogenesis into the infarct border zone (IBZ), tissue perfusion is improved, and the myocardium can be protected from further damage. For maximum therapeutic effect, it is hypothesized that the regenerative substance is best delivered to the IBZ. This requires accurate injections and has led to the development of new injection techniques. To validate these new techniques, we have designed a validation protocol based on myocardial tissue analysis. This protocol includes whole-heart myocardial tissue processing that enables detailed two-dimensional (2D) and three-dimensional (3D) analysis of the cardiac anatomy and intramyocardial injections. In a pig, myocardial infarction was created by a 90-min occlusion of the left anterior descending coronary artery. Four weeks later, a mixture of a hydrogel with superparamagnetic iron oxide particles (SPIOs) and fluorescent beads was injected in the IBZ using a minimally-invasive endocardial approach. 1 h after the injection procedure, the pig was euthanized, and the heart was excised and embedded in agarose (agar). After the solidification of the agar, magnetic resonance imaging (MRI), slicing of the heart, and fluorescence imaging were performed. After image post-processing, 3D analysis was performed to assess the IBZ targeting accuracy. This protocol provides a structured and reproducible method for the assessment of the targeting accuracy of intramyocardial injections into the IBZ. The protocol can be easily used when the processing of scar tissue and/or validation of the injection accuracy of the whole heart is desired.

Video Link

The video component of this article can be found at <https://www.jove.com/video/54974/>

Introduction

Ischemic heart disease has been the world's leading cause of death for the past decades¹. Acute treatment after myocardial infarction aims to restore blood flow to the myocardium via percutaneous coronary intervention or coronary artery bypass grafting. In severe infarctions, a large area of the myocardium is scarred, and these cases often result in ischemic heart failure (HF)². Current treatment options for HF focus on prevention and the preservation of cardiac function for the HF patients, but not on regeneration.

In the last decade, cardiac regenerative therapies have been investigated as a treatment option for HF³. This therapy aims to deliver biologicals, such as stem cells or growth factors, directly to the injured myocardium to induce revascularization, cardiomyocyte protection, differentiation, and growth⁴. For optimal therapeutic effect, it is hypothesized that the biological must be injected in the infarct border zone (IBZ) to facilitate good tissue perfusion for the survival of the biological and for optimal effect to the target zone^{5,6}. Multiple techniques have been developed to perform identification and visualization of the IBZ to guide intramyocardial injections^{7,8,9,10,11}. Besides identification and visualization of the IBZ, the delivery also relies on the biomaterials and injection catheters used. To validate the injection accuracy of the delivery techniques, an accurate and reproducible quantification method is required.

We have developed a protocol for whole-heart myocardial tissue processing that offers two-dimensional (2D) and three-dimensional (3D) imaging, which can be used for qualitative and quantitative study aims. The protocol covers the embedding process and the digital image analysis. In this paper, we demonstrate a protocol for the assessment of the targeting accuracy of intramyocardial injections in the IBZ in a large porcine model of chronic myocardial infarction.

Protocol

The *in vivo* experiment was conducted in accordance with the Guide for the Care and Use of Laboratory Animals prepared by the Institute of Laboratory Animal Research. The experiment was approved by the local Animal Experiments Committee.

1. Preparation of Injectable and Embedding Solution

1. Prepare the injectable gel.
 1. Prepare 1 mL of ureido-pyrimidinone (UPy) gel in accordance to previously-described protocols^{12,13}.
 2. Add superparamagnetic iron oxide particles (SPIOs) to the solution to get a concentration of 15 µg/mL and stir the mixture for 5 min for uniform distribution.
 3. Add the fluorescent microbeads to the solution to get a concentration of 10,000 beads/mL and stir the mixture for 5 min for uniform distribution.
 4. Store the resulting mixture at room temperature in a dark environment. Warm and vortex or stir the solution shortly before the injection procedure.
2. Prepare the embedding solution.
 1. Start with tap water at room temperature and add agarose (agar) to a concentration of 4 wt%.
 2. Slowly heat up the solution to the boiling point using a microwave oven and stir frequently during heating. Upon reaching the boiling point, store and keep the agar solution above 70 °C for 2 h to allow trapped air to surface.
 3. Allow the agar to cool down at room temperature to a temperature between 50 and 60 °C until the time of embedding.

2. Injection Procedure

1. Perform premedication (anti-arrhythmic agents, anti-platelet therapy, and pain medication), anesthesia, venous access, and intubation, as previously described¹⁴.
2. Perform injections using an intramyocardial injection catheter (**Table of Materials**). For each injection, 0.2 mL of the mixture is injected in one bolus at a constant rate of approximately 0.3 mL/min using an injection device. Place the injections at different positions along the IBZ¹².
3. Administer 0.2 mL/kg (1.0 mmol/mL) of a gadolinium-based contrast agent 15 min prior to euthanizing the animal.
4. Administer 20 mL of 7.5% potassium chloride intravenously to euthanize the animal.
5. Secure mediastinal access following protocol steps 8.2 - 8.3, as described by Koudstaal *et al.*¹⁴. Cut the inferior caval vein 5 cm from the right atrium and remove outflowing blood with a suction device. Excise the heart and rinse it with 0.9% saline at room temperature.

3. Embedding Procedure

1. Prepare the heart.
 1. Remove the pericardium from the heart while keeping the atria and ventricles intact. Dissect the ascending aorta ± 1 cm above the aortic valve using Klinkenberg scissors. Cut the inferior caval vein ± 1 cm from the atrium, and do the same for the pulmonary veins.
 2. Suture the apex of the heart to the bottom of a plastic embedding container (17 x 15 x 15 cm, W x D x H) using a 2-0 suture to prevent floatation of the heart during embedding (**Figure 1A**).
 3. Suture the remaining part of the aorta to the rims of the container using 2-0, making sure that the heart is centered and not touching the walls of the container (**Figure 1B**).

Figure 1: Schematic Overview and Photograph of the Embedding Container. (A) Schematic overview of the embedding process. The heart (red) is secured in the container (blue) using sutures. After filling the heart with the agar solution, the space around the heart is filled. Finally, two rigid plastic tubes (yellow) are positioned in the container, next to but not touching the heart, to serve as a reference during image registration. (B) Photograph of a heart secured in the embedding container. The sutures are clamped to the rim of the container using mosquito clamps. [Please click here to view a larger version of this figure.](#)

2. Embed the heart in an end-diastolic-like geometry.

NOTE: The prevention of air bubble creation is necessary. If large air bubbles present in the agar solution, keep the agar at 40 °C, allowing the air bubbles to surface.

 1. Clamp the inferior caval vein using mosquito clamps. Slowly inject the liquid agar using a 50-mL syringe in the right atrium via the superior caval vein until both the right atrium and ventricle are completely filled.

2. Clamp the pulmonary veins using mosquito clamps. Gently pass an agar-filled 50-mL syringe retrogradely through the aortic valves. Slowly inject the solution in the left ventricle (LV) until the LV and the left atrium are completely filled. After filling the LV, clamp the aorta to keep the agar in the LV.
3. Pour the remaining agar into the container until the heart is fully covered. Place two rigid plastic tubes within the embedding container to serve as reference structures for later image registration (**Figure 1A**). Make sure the tubes do not touch the walls of the container or the heart.
4. Let the agar solidify at 2 - 7 °C.

4. Image Acquisition

1. Perform transversal *ex vivo* MRI scans of the heart that is embedded in the container.
 1. Place the container with the embedded heart inside a head coil (**Table of Materials**).
 2. Angulate the slices parallel to the bottom of the container. Use the same orientation and angulation in each *ex vivo* MRI sequence.
 3. To visualize myocardium, perform a fluid-attenuated inverse recovery (FLAIR) sequence with the following parameters: repetition time [TR]/echo time [TE] = 10 s/140 ms, flip angle = 90°, pixel size = 0.5 x 0.5 mm, field of view [FOV] = 169 x 169 mm, 320 x 320 matrix, and 3-mm slice thickness.
 4. To visualize the myocardial infarction, perform a late-gadolinium enhanced (LGE) sequence with the following parameters: [TR]/[TE] = 5.53 ms/1.69 ms, flip angle = 25°, pixel size = 1.0 x 1.0 mm, [FOV] = 169 x 169 mm, 176 x 176 matrix, and 3-mm slice thickness.
 5. To visualize SPIOs, perform a T2*-weighted gradient echo sequence with the following parameters: [TR]/[TE] = 88.7 ms/15 equally-distributed TEs with a range of 1.9 - 24.6 ms, flip angle = 15°, pixel size = 0.5 x 0.5 mm, [FOV] = 169 x 169 mm, 320 x 320 matrix, and 3-mm slice thickness.
2. Tissue processing
 1. Turn the container upside down and allow air between the agar and the sides of the container to remove the solid agar solution, including the heart, from the container. Remove the plastic rods from the solid agar.
 2. Section the agar block containing the heart in 5-mm slices from the apex to the base of the heart using a meat slicer. Keep the angulation of the cut slices the same as in the acquired MR images by cutting parallel to the bottom of the agar block.
 3. Stain the agar slices (including the heart) for 15 min in 1 wt% of 2,3,5-triphenyltetrazoliumchloride (TTC) dissolved in 0.9% saline at 37 °C, and photograph the slices on both sides from a perpendicular view (**Figure 2A**). Next, carefully rinse the slices in 0.9% saline.
NOTE: In this study, we used a DSLR setup with an appropriate lens/objective, a tripod, and uniform lighting. However, the photographs served only as a control for the assessment of the scar region, so we could have used a different setup.
3. Fluorescence imaging
NOTE: Depending on the excitation and emission wavelengths of the fluorescent microbeads, select the appropriate filter block and excitation lasers (e.g., the red microbeads used here have excitation and emission wavelengths of 580 nm and 605 nm, respectively; therefore, the selected excitation laser and bandpass filters were set to 532 nm, 580/30 nm and 610/30 nm, respectively).
 1. Select fluorescence-mode imaging on the variable-mode scanner. Set the photomultiplier tube to 430 V or equivalent and the pixel size to 100 x 100 µm. Select an excitation laser (532 nm) closest to the excitation wavelength of the fluorescent microbeads.
 2. For the first filter block, select a bandpass filter (580/30 nm) that overlaps with the emission wavelength of the injected fluorescence beads (channel 1). Select a bandpass filter for the second filter block (610/30) outside the emission wavelength (channel 2).
NOTE: The second filter block serves as a negative control and to remove auto-fluorescence while keeping the injection sites intact.
 3. Scan both sides of the agar slices in the fluorescence mode of the variable-mode laser scanner using the two channels. Make sure that each slice is completely scanned, including the reference holes.

5. Post-processing

NOTE: The first step in image post-processing is the manual segmentation of the myocardium using in-house developed scripts to trace the endo- and epicardial borders, as well as the injection sites. This is the same for both MRI and fluorescence scans.

1. Segment the myocardium in the MRI scans.
 1. Segment the endocardial and epicardial LV borders on the FLAIR MRI sequence images.
 2. Copy the LV segmentation from step 5.1.1 to the LGE-MRI dataset and segment the scar on the LGE MRI sequence.
 3. Copy the myocardium segmentation from step 5.1.1 to the T2*-weighted dataset and segment the SPIO depositions in the LV myocardium.
2. Process the fluorescence images and perform segmentations.
 1. Load the files obtained from the variable-mode scanner and make a separate image of each cross-sectional heart slice.
 2. Flip the slices that were scanned in base to apex orientation and sort the fluorescence images into a stack for both channels that is oriented from apex to base.
 3. Segment the endocardial and epicardial LV borders on the fluorescence images.
 4. Segment the scar manually on the fluorescence images and use the LGE-MRI scan and the photographs to confirm scar morphology.
 5. Subtract the image stack of channel 2 from the image stack of channel 1 to exclude auto-fluorescence. Manually segment the fluorescent microbead depositions and use the T2* images for confirmation.
3. To create an anatomically-correct 3D geometry, perform a rigid registration of the slices in the image stack based on the reference structures (the holes created by the rigid tubes). Calculate and store the applied translation and rotation of each image.

4. Apply the stored transformations to the image stacks and the segmentations. Linearly interpolate the segmentations of both sides of the slices to reconstruct the original slice thickness and to create a 3D model of the data.

6. Analysis

1. Perform 2D and/or 3D measurements of the distance between the centers of the injection sites and the IBZ to assess the injection accuracy. Measure the distance along the endocardial border of the LV segmentation. In **Figure 2C** and **2F**, an example of the 2D and 3D measurements is indicated by the red line.

Representative Results

Tissue Embedding

Through the embedding process, an end-diastolic-like geometry was established. The agar successfully adhered to the heart tissue, enabling the tissue to be sliced at the desired angulation with equal slice thicknesses (**Figure 2A** and **2C**).

Scar- and Injection-site Assessment

For each imaging modality, infarct and injection location assessments were performed successfully. In both 2D fluorescence imaging and MRI imaging, the scar and injection sites were clearly distinct (**Figure 2C**, **2D**, and **2E**, respectively). Photographs of the TTC-stained tissue and LGE-MRI images provide a control for scar assessment in fluorescence imaging (**Figure 2A** and **2C**).

3D Reconstruction

The reference markers provide an accurate and reliable method for image registration. Image post-processing enables the reconstruction of the 3D geometry of the *ex vivo* heart based on the segmentations and the fluorescent images of the heart (**Figure 2F**). The 3D geometry of the segmentations allows for an accurate 3D injection accuracy assessment (**Figure 2F**).

Measurements

In this study, the injection depositions and IBZ were projected onto the endocardial wall. Afterwards, the distances between the projections on the endocardial surface were measured (**Figure 2C** and **2F**). The high-resolution (0.1 x 0.1 mm) fluorescent images allowed accurate measurements. In the 3D reconstruction, the resolution in the z-direction due to the slice thickness was 2.5 mm.

Figure 2: Typical *Ex Vivo* Imaging Data and 3D Reconstruction. The resulting images acquired by the different modalities used in this protocol. All images show the same transverse slice of the embedded heart. **(A)** Photograph of the TTC-stained slice in which the scar is visible. **(B)** Schematic overview of the anatomical structures. **(C)** Fluorescence image with both channels combined. The channel covering the bead emission spectrum is shown in red and the negative control is shown in green. The red circle indicates the injection site. The distance measurement from the injection to the IBZ is indicated with the red line. **(D)** Short-axis LGE-MRI; the infarct area is shown as a hyper-intense white area. **(E)** T2*-weighted MRI; the SPIO particles within the injected substance can be recognized as the local signal void indicated by the red circle. **(F)** 3D visualization of injection sites (red), scar tissue (white), and myocardium (green) as segmented in the fluorescent images. The arrow indicates the same injection spot as in **C** and **E**. In this image, the same distance measurement is indicated with the red line. LV = Left Ventricle, RV = Right Ventricle. The scale bar represents 10 mm. [Please click here to view a larger version of this figure.](#)

Discussion

Whole-heart 3D myocardial tissue processing according to this protocol provides a structured method that enables the 3D analysis of the infarct, the IBZ, and the performed injections with respect to the cardiac anatomy. The filling volume of the heart depends on the desired analysis. In this study, to assess the injection accuracy, we aimed to fill the heart to resemble the end-diastolic geometry as closely as possible. To enforce this, the LV apex is fixed to the bottom of the container and the LV is filled with agar while the pulmonary veins are clamped. When the LV

is filled, the aorta is clamped as well, preventing the agar from flowing out of the LV and imitating the end-diastolic geometry as closely as possible. Sectioning the embedded heart offers the benefit of uniform slice thickness and allows the slices to be in the same angulation as in *ex vivo* imaging. After slicing, the embedding material prevents the tissue from deformation caused by the handling of the slices during image acquisition. Ideally, TTC staining should be performed as soon as possible after removal from the body, as the staining relies on enzymes to differentiate between metabolically-active and -inactive tissues. In our protocol, however, there are several important steps that must be performed before the TTC staining can take place, including the embedding process, in which the embedded heart is cooled to solidify the agar. Since we have observed clear staining of the infarcted tissue in all slices, we believe that this effect was minimal.

The imaging equipment used here can be replaced by different equipment that provides the same functionality. High-resolution fluorescence imaging on a variable-mode laser scanner and the option to set multiple filter blocks in order to effectively and accurately process the tissue are essential for detailed analysis. For image post-processing, software packages that allow full freedom to perform image analysis are required. In our experience, 3D analysis for the assessment of the injection accuracy was used, but analysis on the 2D images is also possible.

We have thus far performed this myocardial tissue processing method in 10 pigs and have been able to find 73% of the injection sites of in a total of 118 performed injections. The difference between the amount of injections performed and the amount of identified injection sites is possibly caused by the difference between the 5-mm slice thickness and the 1.5-mm penetration depth of the fluorescence scanner. Theoretically, 2 mm of tissue is not measured in each slice. Thinner slices would solve this problem.

Limitations

Despite the end-diastolic-like geometry at the start of the embedding process, some hearts appeared to have contracted a little in the agar. Since we observed no large deviations from the end-diastolic volume, we believe that this effect was minimal and did not affect the injection accuracy assessment. Using thinner tissue slices would improve the accuracy of the assessment and allow for a more detailed comparison with *ex vivo* MRI. Another option would be to use NIRF agents instead of fluorescent microbeads to improve the penetration depth and possibly-detected fraction. Furthermore, the low temperature of the embedded heart and the timing of the TTC staining might cause a lack of the enzymes that are necessary for this type of staining. Nevertheless, the photographs of the stained slices proved to be a good control for scar assessment.

Future perspectives

Although this method was originally designed for accuracy assessments of intramyocardial injections, studies with other endpoints can also benefit from this method (*e.g.*, infarct size, morphology assessment, or other organs). In addition to MRI, other 3D imaging modalities, such as CT, PET, or SPECT, can be used on the myocardial tissue following the demonstrated methodology. In addition, the integration of these different imaging modalities could possibly further optimize the 2D and 3D analyses.

Conclusion

To conclude, we have provided a novel, standardized, and reproducible method to perform 3D whole-heart myocardial tissue processing. Agar has proven to be a suitable medium for whole-heart embedding, enabling the tissue to be sliced at the desired angulation and with equal thickness. Moreover, the image registration proved feasible for the 3D reconstruction of myocardial imaging, enabling 3D assessment at a high spatial resolution, which can be used for qualitative and quantitative study aims.

Disclosures

The authors have nothing to disclose.

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