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Ligand electronic properties modulate tau filament binding site density

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Abstract

Small molecules that bind tau-bearing neurofibrillary lesions are being sought for premortem diagnosis, staging, and treatment of Alzheimer's disease and other tauopathic neurodegenerative diseases. The utility of these agents will depend on both their binding affinity and binding site density ($B_{\max}$). Previously we identified polarizability as a descriptor of protein aggregate binding affinity. To examine its contribution to binding site density, we investigated the ability of two closely related benzothiazole derivatives ((E)-2-[[4-(dimethylamino)phenyl]azo]-6-methoxybenzothiazole) and ((E)-2-[2-[4-(dimethylamino)phenyl]ethenyl]-6-methoxybenzothiazole)) that differed in polarizability to displace probes of high (Thioflavin S) and low (radiolabeled (E,E)-1-iodo-2,5-bis(3-hydroxycarbonyl-4-methoxy)styrylbenzene; IMSB) density sites. Consistent with their site densities, Thioflavin S completely displaced radiolabeled IMSB, but IMSB was incapable of displacing Thioflavin S. Although both benzothiazoles displaced the low $B_{\max}$ IMSB probe, only the highly polarizable analog displaced near saturating concentrations of the Thioflavin S probe. Quantum calculations showed that high polarizability reflected extensive pi-electron delocalization fostered by the presence of electron donating and accepting groups. These data suggest that electron delocalization promotes ligand binding at a subset of sites on tau aggregates that are present at high density, and that optimizing this aspect of ligand structure can yield tau-directed agents with superior diagnostic and therapeutic performance.

Keywords

Alzheimer's disease; tau protein; ligand binding; polarizability; dispersion forces; computational chemistry

1. Introduction

Tauopathic neurodegenerative diseases, including Alzheimer's disease (AD) and certain forms of frontotemporal lobar degeneration, are characterized by the appearance of tau-aggregate bearing neurofibrillary lesions in characteristic brain regions (reviewed in [1]). The tau aggregates adopt filamentous morphology reflecting their underlying cross- β -sheet

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structure (*i.e.*, parallel in register β -sheets oriented perpendicular to the filament long axis) [2]. Because the spatial and temporal distribution of tau aggregates correlates with disease progression, they can be used to differentially diagnose and stage tauopathies in postmortem samples (reviewed in [3, 4]). In addition to being useful biomarkers, tau aggregates are potential mediators of neurodegeneration owing to toxicity associated with their accumulation [5]. Thus, tau aggregates also are promising targets for drug discovery efforts.

To date, the search for ligands capable of binding filamentous tau aggregates has focused on affinity, resulting in the identification of compounds with K_d s in the low- to mid-nanomolar range [6, 7]. However, the utility of candidate compounds also will depend on binding site density ($B_{\max}$). For example, the signal generated by whole-brain imaging agents is proportional to B_{avail}/K_d ratio, or “binding potential”, where B_{avail} (*i.e.*, the concentration of available binding sites *in vivo*) is a function of both target concentration and $B_{\max}$ [8]. Thus, occupancy of high density sites can be important for detection of low abundance targets *in vivo*. In fact, the binding potential needed for putative tau imaging agents will likely be higher than for established amyloid radiotracers owing to the low molar concentration of the tau binding target in diseased brain relative to A β aggregates [9]. Ligand $B_{\max}$ also may be important for tau filament-directed therapeutics. For example, one strategy for preventing toxicity involves blocking aggregate surfaces with molecular coatings [10, 11]. High $B_{\max}$ ligands would be preferable for maximizing the efficacy of this approach.

Despite its importance, little is known about binding site density on protein aggregates, except that substantial variability exists among individual ligands. For example, the presence of at least three binding modes on A β filaments that differ in $B_{\max}$ has been reported [12]. In the case of tau aggregates, $B_{\max}$ has been reported to vary over the range of 0.001 – 0.05 mol/mol (*i.e.*, 1:1000 – 1:20 mol ligand/mol tau protomer), suggesting that a wide range of binding site densities appear on tau filaments too [6, 13, 14]. Although structure activity analysis has revealed structural features on certain scaffold classes that mediate binding affinity [15, 16], descriptors associated with individual modes of interaction remain poorly understood.

To better characterize the interaction between small molecules and cross- β -sheet aggregates, we have turned to benzothiazole derivatives as model ligands and quantitative structure activity relationship analysis as a means to identify their binding descriptors. Using this approach, we identified ligand polarizability as a descriptor of thioflavin dye displacement potency from synthetic cross- β -sheet aggregates composed of insulin and A β [17]. Polarizability, which describes how easily electron density can shift about a molecule when exposed to an external electric field, reflects underlying electron delocalization [18]. We then found that the correlation between ligand polarizability and thioflavin dye displacement potency extended to synthetic tau aggregates as well [19]. Interestingly, as thioflavin probe concentrations rose, the displacement *efficacy* of weakly polarizable ligands was greatly attenuated whereas the efficacy of highly polarizable ligands was unchanged [19]. These data suggested that binding site occupancy varied with probe concentration, and that ligand polarizability was a potential descriptor for binding sites occupied as probe neared saturation (corresponding to high $B_{\max}$ sites). Consistent with this possibility, an ^{18}F -labeled analog of one of most highly polarizable benzothiazole analogs in our series, (E)-4-((6-(2-(2-(2-fluoroethoxy)ethoxy)ethoxy)benzo[d]thiazol-2-yl)-diazanyl)-N,N-dimethylaniline (FPPDB), has achieved the highest $B_{\max}$ yet reported for a synthetic tau filament binding agent (~1:20 tau protomer:ligand ratio) [13].

Here we examine the relationship between ligand polarizability and site occupancy using two closely related benzothiazole derivatives as ligands, and both synthetic and authentic disease derived tau filaments as binding targets. The results indicate that incorporation of

polarizability considerations into ligand design may yield agents with superior diagnostic and therapeutic performance.

2. Materials and Methods

2.1. Materials

Octadecyl sulfate (ODS) was from Research Plus (Bayonne, NJ), ThT, ThS (CAS registry 1326-12-1), Congo red (ultrapure grade) was from Anaspec (Fremont, CA), and compounds **1** and **2** were custom synthesized as described [20]. Both ^{125}I -radiolabeled (in 40% ethanol) and unlabeled (*E,E*)-1-iodo-2,5-bis(3-hydroxycarbonyl-4-methoxy)styrylbenzene (IMSB) [21] were the generous gifts of Avid Pharmaceuticals (Philadelphia, PA).

Recombinant human His₆-2N4R tau protein was prepared as described previously [22]. Synthetic tau filaments were prepared from recombinant protein (5 μM) incubated (24 h at 37°C) in assembly buffer (10 mM HEPES, pH 7.4, 100 mM NaCl, 5 mM dithiothreitol) in the presence of 50 μM ODS inducer [7, 23], and stored in aliquots at -80°C until used.

Authentic paired helical filament (PHF) tau was prepared from AD brain as described previously [19]. The tau content of PHF preparations was determined by dot blot using recombinant 2N4R-tau as standard. Aliquots were diluted in 0.1% SDS and 0.1% 2-mercaptoethanol, then spotted in triplicate onto 0.2 μM nitrocellulose membranes. After blocking in 4% nonfat dry milk, blots were developed using monoclonal antibody Tau5 as described previously [24]. PHF-tau weights were converted to moles assuming a mean molecular mass of 40,238 g/mol, which reflects the estimated ratios of all six human isoforms [25, 26].

2.2. Filament length distributions

Filament populations were viewed and digitally captured on a Tecnai G2 Spirit BioTWIN transmission electron microscope (FEI, Hillsboro, OR) operated at 80kV and 68,000 $\times$ magnification. Filament lengths were measured using ImageJ software (National Institutes of Health) and segregated into bins as described previously [27]. Length distributions were fit to the log normal function:

$$y = ae^{\left[-0.5\left(\frac{\ln(x/x_0)}{b}\right)^2\right]} \quad (\text{eq 1})$$

where y is the number of filaments per bin of length interval midpoint x , a is the number of filaments per bin at distribution mode x_0 , and b is an estimate of distribution skew.

2.3. Fluorescence displacement assays

ThS fluorescence assays were performed as described previously [7]. Synthetic 2N4R-tau and authentic PHF-tau filaments (1 μM total tau concentration) were incubated (2 h at 37°C) in assembly buffer with varying concentrations of ThS probe ($1.7 \times 10^{-11} - 10^{-5}$ M) and test ligand ($0 - 10^{-5}$ M). Fluorescence was measured using a FlexStation microplate reader (Molecular Devices, Sunnyvale, CA) at $\lambda_{\text{ex}} = 440$ nm; $\lambda_{\text{em}} = 490$ nm; filter = 475 nm. Thioflavin dye displacement (net fluorescence) was determined by subtracting no protein controls from protein and compound fluorescence readings. Net fluorescence readings were normalized to percent displacement using no compound controls.

2.4. Radioligand binding assays

^{125}I IMSB binding and displacement from tau filaments were assessed using a filter trap assay [12, 28]. Tau filaments (230 nM synthetic 2N4R-tau; 300 nM authentic PHF-tau) were

incubated (4 h at 37°C with hourly agitation) with varying concentrations of [¹²⁵I]IMSB and ligand in PBS buffer (10 mM Na₂HPO₄/KH₂PO₄, 137 mM NaCl, 2.7 mM KCl, pH 7.4). For determination of nonspecific binding, ligand was replaced with 8 μM of Congo red. Aliquots were then vacuum filtered (5 – 10 s) over glass fiber filters (0.3 μm pore diameter, Sterlitech) in a Millipore 1225 Sampling Manifold using a Pharmacia LKB VacuGene Pump operated at 50 mbar. Each sample was then washed four times with 3-ml volumes of PBS. Filters were collected in polypropylene tubes and counted using a Packard A5003 gamma counter (Packard Instrument Company, Meriden, CT) with 84% efficiency. [¹²⁵I]IMSB specific binding was determined by subtracting nonspecific binding from total binding. Under these assay conditions, the specific binding signal accounted for ~80% of the total radioactivity.

2.5. Spectrophotometry

Absorbance spectra were collected in methanol solvent using a CARY50Bio UV-VIS spectrophotometer and recorded with the Cary WinUV Scan Application version 3.00(182). Spectra were fit to a double Gaussian function as described previously [29].

2.6. Analytical methods

Binding and displacement potencies of ligands in radioactivity and fluorescence assay formats were determined from the function:

$$F = F_{\min} + \frac{F_{\max} - F_{\min}}{1 + (x/AC_{50})^n} \quad (\text{eq 2})$$

For direct binding assays, F represents the net signal at concentration x of probe, $F_{\min}$ is the signal at zero probe concentration, $F_{\max}$ is the net signal at infinite probe concentration, n is the Hill coefficient, and AC_{50} corresponds to probe K_d . For displacement assays conducted at constant probe concentration, F represents the probe signal in the presence of varying concentrations of test ligand, $F_{\min}$ is the signal at infinite ligand concentration, $F_{\max}$ is the signal in the absence of test ligand, AC_{50} is the concentration of test compound that reduces probe signal by 50%.

2.7. Computational chemistry

Quantum property calculations were performed using density functional theory methods implemented in Gaussian 09 (G09) [30] and Turbomole V6.3.1 [31] software packages available on Ohio Supercomputer Center clusters. All calculations were performed using hybrid density functional B3LYP and the 6-311++G(d,p) basis set, which together have been reported to accurately model photophysical properties of dye molecules in implicit solvent [32].

Dipole moments were calculated in G09 after optimizing ground state geometries using G09 as described previously [17] and excited state calculations for $\lambda_{\max}$ were performed using time-dependent density functional theory (TD-DFT) method (G09 keyword TD=NStates=3). Electrostatic potential surface calculations were performed on compound ground-state geometries using population analysis with atomic charge assignments produced according to the ChelpG scheme [33] (G09 keyword pop=chelpg) as implemented in G09. Surface plots were generated in GaussView 4.1.2 by mapping electrostatic potentials onto SCF (self consistent field) total density surfaces with isodensity contour values of ± 0.0004 a.u. To facilitate direct comparison between compounds, electrostatic potential energy scales were normalized to a standard color scale (± 55.8 kcal/mol) such that all potentials resided within the standard extremes. For all G09 calculations, bulk solvent effects were implicitly

modeled with the polarizable continuum model [34] (G09 keywords SCRF =(Solvent = Methanol)).

Electronic difference density calculations were performed in Turbomole for first excited (S_1) and ground states (S_0) on compound ground-state geometries under C_1 molecule symmetry (control keywords \$scfinstab and \$soes) as implemented in the Turbomole egrad module. Because this module does not implement implicit solvent effects, these calculations were performed in gas phase. Electronic difference maps were generated using UCSF Chimera Alpha Version 1.5 (build 31329) [35] software with isodensity contour values ± 0.004 a.u. Contour volumes were measured using Chimera's Volume tool.

The calculated log octanol/water partition coefficient (clogP) and molecular volume were calculated with the Molinspiration Property Calculation Service (www.molinspiration.com).

3. Results

3.1. Tau filament populations for binding studies

Synthetic filaments composed of recombinant 2N4R-tau were prepared to investigate ligand binding properties. The 2N4R isoform was chosen because it efficiently aggregates *in vitro* and has been used in previous investigations of ligand binding [7, 13, 19]. Tau filaments prepared from AD brain also were prepared so that interaction with authentic aggregates could be compared. These filaments differed from synthetic filaments by being composed of all six central nervous system isoforms and by containing extensive post-translational modifications (reviewed in [1]). Both preparations displayed clear filamentous character when viewed in transmission electron micrographs (Figure 1A,B). However, they differed in morphology, with synthetic filaments displaying straight morphology whereas the authentic filaments retained the classic morphology of PHF (Figure 1A,B). Moreover, the two filament populations differed in length distribution. The PHF population averaged 193 nm in length and displayed a clear mode at 123 ± 2 nm when fit to a log-normal distribution (Figure 1C). These dimensions, which were consistent with literature values for filaments isolated by differential centrifugation [36], reflect the effects of breakage and shearing during isolation. In contrast, synthetic 2N4R-tau filaments averaged 776 nm in length and were predicted on the basis of a log-normal distribution to have a mode within the standard error of estimate of zero (Figure 1C). These data indicate that synthetic filament length distribution was skewed toward longer lengths relative to PHFs.

3.2. Displacement Probes

To characterize the binding surfaces presented by tau filaments, the interaction of each filament preparation with fluorescent thioflavin dyes (ThT and ThS)[37] and radioprobe [125 I]IMSB [21] was investigated. These compounds were chosen as binding probes because they had been reported to bind tau-bearing neurofibrillary lesions in brain sections [38, 39] yet differed substantially in structure. For example, the major component of ThS adopts a donor- π -acceptor (D- π -A) configuration, composed of strong benzothiazolium electron acceptors linked to a strong dimethylamine electron donor through a planar conjugated π network (Table 1). In contrast, IMSB has two weak methoxy electron donors feeding into a conjugated aromatic π network yielding a donor- π -donor (D- π -D) configuration (Table 1). As a result, ThS was a colored compound with a strong absorbance maximum at 377 nm and a weak shoulder at 420 nm, whereas IMSB appeared colorless with an absorbance maximum centered at 350 nm (Figure 2). Overall, ThS and IMSB probes were charged molecules of similar size and shared planar, highly conjugated organization (Table 1). However, they differed in hydrophobicity and electronic structure, especially in the magnitude of delocalization of their π electron systems.

When assayed in filter trap format (300 nm pore diameter) at constant tau protomer concentration, both 2N4R aggregates and PHF-tau bound [125 I]IMSB with affinities estimated in the low nanomolar range (Figure 3A). However, $B_{\max}$ was only $1:112 \pm 25$ ([125 I]IMSB:tau) for 2N4R tau and $1:2990 \pm 160$ ([125 I]IMSB:tau) for PHF. Because the percentage of total aggregation distributed into filaments 300 nm in length was higher for synthetic filaments (90%, Figure 1C) than for PHFs (31%, Figure 1C), a portion of the observed $B_{\max}$ difference may have resulted from differences in filament length distribution. However, the majority of the 23 ± 2 fold difference in $B_{\max}$ reflected a lower density of high affinity IMSB sites on PHFs relative to synthetic filaments.

When synthetic filaments were assayed in fluorescence format with near saturating concentrations of ThS and ThT, both probes underwent excitation and emission Stokes shifts and fluoresced brightly (Figure 3B). These results were consistent with previous reports [40]. However, only ThS fluoresced strongly in the presence of PHF, with ThT fluorescence intensity being 15 ± 1 fold lower than in the presence of equimolar concentrations of 2N4R filament protomer (Figure 3B). To maintain tau protomer concentrations at similar levels for interaction assays involving synthetic and authentic filaments, all subsequent studies involving thioflavin dye probes used ThS exclusively.

To clarify the relationship between IMSB and ThS sites, the ability of probes to displace each other was investigated. Despite its high binding affinity, IMSB proved incapable of displacing ThS from either synthetic tau filaments (Figure 4A) or authentic PHF-tau (Figure 4B) by 50% when present at saturating concentrations up to 10 μ M. In contrast, ThS completely displaced [125 I]IMSB from synthetic filaments with AC_{50} of 249 ± 60 nM (Figure 5). Together these data indicated that IMSB and ThS differentially interacted with tau filaments, with IMSB selectively probing low density sites capable of supporting high affinity binding. In contrast, ThS interacted with IMSB sites but also additional sites that were present at similar densities on both PHF and synthetic filaments.

3.3. Benzothiazole ligands differentially displace IMSB and ThS probes

To further characterize IMSB and ThS modes of interaction, the ability of neutral benzothiazole derivatives **1** and **2** (Table 1) to displace each probe was investigated. The two ligands differed only by the structure of the bridge that connected the benzothiazole and aryl moieties: **1** contained an azo bridge whereas **2** contained an alkene bridge. As a result, the two compounds shared similar size, hydrophobicity and neutral net charge (Table 1). Nonetheless, bridge structure greatly affected compound absorbance, with compound **1** appearing red and having an intense lowest energy charge-transfer absorption band centered at 508 nm whereas **2** appeared yellow and absorbed at 393 nm (Figure 2B). Consistent with previous results [20], **1** efficiently displaced ThS probe from synthetic 2N4R filaments with an AC_{50} of 31 ± 6 nM (Figure 4A). In contrast, **2** did not displace ThS by 50% at concentrations up to 10 μ M. A similar pattern was observed for ThS displacement from PHF, where **1** displaced ThS with AC_{50} of 48 ± 4 nM and **2** displaced with $AC_{50} > 10$ μ M (Figure 4B). These data indicate that **1** had far greater ability than **2** to interact with binding sites occupied by ThS, and that this pattern of interaction held for authentic PHFs as well as for synthetic filaments.

On the basis of ThS probe displacement described above, compound **2** appeared to bind poorly to tau filaments. Yet when tested in [125 I]IMSB competition format, **1** and **2** both displaced probe with similar affinity (AC_{50} s of 29 ± 6 and 45 ± 11 nM, respectively), and with nearly equal efficacy (Figure 5). These data reveal that both **1** and **2** were capable of binding tau filaments with high affinity at the low density sites bound by IMSB, but that they differed greatly in their ability to bind the additional sites occupied by near saturating concentrations of ThS probe.

3.4. Electronic properties of tau aggregate binding ligands

To characterize their electronic properties, the *E* geometric isomers of **1** and **2** (shown in Table 1) were analyzed using a quantum chemical modeling approach. First, the ground state geometries of **1** and **2** were optimized in polar solvent at the B3LYP/6-311++G(d,p) level of theory. To test the quality of the models, $\lambda_{\max}$ and oscillator strength corresponding to vertical excitations S1, S2, and S3 were calculated and compared to experimental values. The calculations predicted that the S1 state far exceeded S2 and S3 in oscillator strength for both compounds (Table 2). Indeed, experimental values for $\lambda_{\max}$ were in general agreement with values calculated for the $S_0 \rightarrow S_1$ excitation for both compounds (Table 2). However, $\lambda_{\max}$ for **2** was slightly overestimated in the calculation, potentially reflecting greater rotational freedom of its dimethylamine moiety [41, 42].

Second, to assess overall compound polarity in the ground state, calculated molecular electrostatic surface potentials were mapped onto electron density isosurfaces and plotted along with dipole moment. Both compounds presented electronegative surfaces along the faces of their conjugated π systems (Figure 6A). However, for compound **1**, negative electrostatic potential localized most intensely on the nitrogen atoms of the benzothiazole heterocycle and azo bridge, with positive electrostatic potential localized primarily on the dimethylamine electron donor group. This pattern was consistent with extensive delocalization of electrons through the conjugated π system from donor groups toward thiazole and azo group nitrogen atoms. The resulting separation of negative and positive charges created a permanent ground state dipole moment of 7.8 D oriented approximately parallel to the compound long axis (Figure 6A). In contrast, compound **2** supported lower charge polarity, with localized negative charge being limited to the nitrogen atom of the benzothiazole moiety (Figure 6A). As a result, ground state dipole moment decreased 30% relative to **1**. These data indicate that the azo bridge fostered more effective coupling between electron donor and acceptor groups than the alkene bridge, resulting in more charge transfer character in the ground state of **1** relative to **2** in polar solvent. Proposed resonance forms that contribute to charge transfer character are shown in Figure 6B.

Finally, to model how bridge composition affected electron movement to higher energy states, vertical excitations were calculated for **1** and **2** at the B3LYP/6-311++G(d,p) level of theory and used to compute differences in electron density between the ground (S_0) and lowest identified singlet excited states (S_1). Analysis was limited to gas phase owing to computational constraints. The resultant $S_1 - S_0$ difference maps identified the locations of electron density that dispersed from the ground state and accumulated upon excitation to the higher energy level (Figure 7). The $S_1 - S_0$ difference density map for **2** exhibited a change in electron density that alternated in sign along the conjugated alkene bridge, which is characteristic of a (π, π^*) excited state. Electron density on the methoxy and dimethylamine donors shifted further toward the thiazole ring in the excited state. In contrast, the $S_1 - S_0$ difference density map for **1** was dominated by the depletion of electron density from the lone pairs of the bridge nitrogen atoms, implicating a (n, π^*) excited state. Electron density redistributed toward the thiazole and phenyl ring systems and within the bridge. Overall, the difference maps showed that the volume of perturbed density was 1.7-fold greater for **1** relative to **2** (on the basis of identical isocontouring), consistent with increased charge transfer efficiency in this compound. Together these calculations show that simple replacement of the alkene bridge in **2** with an azo moiety to create **1** altered compound electronic properties by enhancing electron delocalization in the ground state and by supporting greater intramolecular charge transfer in response to photoexcitation. These characteristics, which were fostered while holding compound hydrophobicity, size, and net charge nearly constant, correlated with increased displacement efficacy against sites occupied by ThS probe relative to those occupied by the IMSB probe.

4. Discussion

These data show that the efficacy of probe displacement from tau filaments is highly sensitive to the electronic properties of ligand. Importantly, they show that displacement of near saturating concentrations of ThS probe, which occupies sites over and above those occupied by IMSB, can be selectively enhanced by fostering a highly delocalized electronic structure. Thus, they suggest a route for rationally maximizing the binding potential of imaging radiotracers and the efficacy of interaction-inhibiting molecular coatings [10, 11]. Because PHF-tau shares this behavior with synthetic 2N4R-tau filaments, the route can yield ligands with utility for human disease. Because electronic properties can be modulated in small molecules while maintaining zero net charge, the proposed strategy is consistent with the need to maintain blood brain barrier penetrability of ligands for diagnostic and therapeutic applications.

A role for electronic structure in mediating filament binding is consistent with recent models of small molecule/cross- β -sheet aggregate interactions formulated on the basis of docking [43, 44] and molecular dynamics simulation [45–47]. These computational models predict that binding occurs in shallow channels oriented parallel to the long filament axis formed by solvent exposed amino acid side chains. Thus, potential binding sites are predicted to vary with the dimensions of the channels and their surface chemical properties (*e.g.*, amino acid side chain composition). The most energetically favorable interactions identified involved Phe residues, which presented a surface composed of aromatic moieties, and Gly residues, which exposed the delocalized π system of the cross- β -sheet main chain core [44, 46]. In the case of compounds investigated herein, two modes of binding with tau aggregates could be discerned. The first mode, which we call Class I, is characterized by high affinity but low $B_{\max}$ binding. Class I activity is shared by diverse structures composed of planar and highly conjugated ring systems that present π -electron rich surfaces, including all four of the probes and ligands investigated herein. Their π -electron systems can but need not be highly delocalized, and as a result these compounds are frequently colorless (*e.g.*, IMSB). The location of their binding sites on tau aggregates is not established, but π -rich heterocycles have been reported to support cation- π , π - π , and CH- π interactions (reviewed in [48]). A tau-aggregate directed radiotracer with Class I electronic character currently undergoing clinical development, THK523 [6], shares a D- π -D electronic organization with IMSB. Although it binds synthetic tau aggregates with a low nanomolar K_d , its $B_{\max}$ is only 0.002 mol/mol (*i.e.*, one ligand molecule for every 460 tau protomers). This binding site density is within ~4-fold of IMSB, but >20-fold lower than FPPDP, an analog of **1**. On the basis of mathematical modeling, we have predicted that this combination of binding parameters (*i.e.*, binding potential) will have difficulty overcoming nonspecific background associated with whole-brain imaging [9]. Imaging performance will be weaker still if, as shown here for [125 I]IMSB, $B_{\max}$ for authentic PHF is lower than for synthetic tau filaments.

In contrast, the second binding mode, which we term Class II, is shared by compounds comprising planar and highly conjugated π systems flanked by electron donor and acceptor groups [19]. As a result, these compounds, which can be intensely colored (*e.g.*, compound **1**), have more highly delocalized electrons in the ground state and greater electron mobility in response to photoexcitation than Class I compounds. These electronic characteristics are ideal for supporting attractive van der Waals interactions with flat binding surfaces on tau and other protein aggregates (reviewed in [49]). Conversely, Class I compounds lack this feature and displace Class II ligands poorly. We propose that this mode of interaction is responsible for the high binding site densities associated with a radiolabeled derivative of **1** [13], which was reported to bind synthetic tau aggregates with $B_{\max}$ up to one order of magnitude greater than Class I compounds [125 I]IMSB (reported herein) or [18 F]THK523 [6]. On the basis of mathematical modeling, we predict that this $B_{\max}$ (when accompanied

by low nanomolar affinity) is adequate for whole-brain imaging applications [9]. Moreover, we have reported that compound **1**, but not **2**, is capable of blocking toxicity associated with tau aggregation in a biological model of tauopathy [50]. Together these data suggest that the Class II mode of interaction offers translational opportunities for tauopathic neurodegenerative diseases.

Our reported quantitative structure activity relationship analysis of benzothiazole derivatives [17], along with quantum chemistry analysis of compounds **1** and **2** reported herein, provide insight into the structural features associated with Class II activity. The most important feature is the introduction of electron acceptor and donor moieties that foster electron delocalization. In the case of **1**, this was achieved by placing an azo bridge adjacent to the weak benzothiazole acceptor in a conjugated π system flanked by electron donating groups. The resulting D- π -A- π -D architecture strongly enhanced intramolecular charge transfer, leading to extensive π electron delocalization in the ground state and lower energy requirements for transition to the first excited state. The resulting increase in dipole moment and polarizability in **1** relative to **2** reflect these features. The dispersion effects supported by this architecture may be especially important for high density binding to tau aggregates, which contain multiple Gly and aromatic residues in their folded core [51]. Nonetheless, compound **1** does not discriminate between A β and tau on the basis of ThS displacement activity [7], and this has been confirmed by direct radiobinding assays [13]. It remains to be seen whether Class II interactions can be harnessed to drive selectivity among protein aggregates composed of different protein protomers.

In summary, here we found that highly delocalized electronic structure fostered potent displacement of cross- β -sheet binding probes from tau aggregates, but only from a subset of binding sites marked by near-saturating concentrations of ThS probe. The high density nature of the sites, combined with the compatibility of delocalized electronic structure with overall neutral compound charge, suggests a route for optimization of binding properties for diagnostic and therapeutic applications.

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Highlights

- Displacement of binding probes from synthetic tau aggregates was investigated.
- Displacement efficacy correlated with ligand polarizability
- Polarizability increased with ligand intramolecular charge transfer efficiency.
- Ligand polarizability is a descriptor of tau-filament binding site density.

Fig. 1. Tau filament morphology and length distribution

Transmission electron microscope images of negatively stained *A*, synthetic filaments composed of 2N4R-tau and *B*, authentic tau filaments purified from AD brain were captured at 68,000-fold magnification. Synthetic filaments adopted straight morphology, whereas authentic filaments adopted classic paired helical morphology. *C*, the dimensions of all filaments 50 nm in length measured from electron micrographs were plotted as the fraction of total filament number that segregated into consecutive length intervals (total filament number $n = 247$ and 111 for 2N4R- and PHF-tau, respectively), whereas each line represents the best fit of data points to a log normal function (eq 1). The length distribution of synthetic 2N4R filaments skewed toward longer lengths relative to the PHF population.

Fig. 2. Optical properties of probes and ligands

Experimental absorption spectra for *A*, probes ThS and IMSB and *B*, ligands **1** and **2** were determined in methanol solvent. Each point represents absorbance normalized for cuvette pathlength and compound concentration (*i.e.*, extinction coefficient) plotted as a function of wavelength (λ). See text for details.

Fig. 3. Probe interactions with filamentous 2N4R- and PHF-tau

A, binding of radioprobe [¹²⁵I]IMSB was determined after incubation with synthetic and paired helical tau filaments. Each point represents specific binding as a function of total [¹²⁵I]IMSB concentration $\pm$ SD (triplicate determination), whereas the lines represent the best fit of the data points to a binding isotherm (eq 2). [¹²⁵I]IMSB bound to both synthetic and paired helical filaments with low nanomolar affinity. ***, $p < 0.001$; n.s., $p > 0.05$ for each comparison. **B**, probes ThS (7.5 μ M) and ThT (1 μ M) were incubated with tau filaments composed of 2N4R- and PHF-tau (each at 1 μ M), then subjected to fluorescence measurements at $\lambda_{ex} = 440$ nm, $\lambda_{em} = 490$ nm. Each bar represents net fluorescence yield associated with binding $\pm$ SD (triplicate determination). ThS fluoresced strongly in the

presence of both 2N4R filaments and PHFs, whereas ThT fluoresced most strongly in the presence of 2N4R filaments.

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Fig. 4. ThS displacement assays for tau filament binding

A, synthetic 2N4R-tau filaments and *B*, PHFs (both at 1 μ M) were incubated with fluorescent ThS probe (7.5 μ M) in the presence of varying concentrations of **1**, **2**, and unlabeled IMSB, then subjected to fluorescence measurements at $\lambda_{\text{ex}} = 440$ nm, $\lambda_{\text{em}} = 490$ nm. Each point represents mean net ThS fluorescence (*F*) (expressed as % fluorescence in the presence of vehicle alone) whereas the solid lines reflect best fit of data points to eq 2. Only compound **1** decreased ThS fluorescence from both filament populations at submicromolar concentrations under these conditions.

Fig. 5. [^{125}I]IMSB displacement assays for tau filament binding

Binding of radioprobe [^{125}I]IMSB to synthetic 2N4R-tau filaments ($1\ \mu\text{M}$) was determined after incubation in presence of varying concentrations of **1**, **2**, and ThS. Each point represents specific binding (expressed as % specific binding in the presence of vehicle alone) as a function of total ligand concentration $\pm$ range (duplicate determination), whereas the lines represent the best fit of the data points to eq 2. All three compounds displaced [^{125}I]IMSB specific binding under these conditions.

Fig. 6. Ligand electrostatic potential surfaces

A, plots for **1** and **2** were generated at the B3LYP/6-311++G(d,p) level of theory and visualized in GaussView 4.1.2. The semi-transparent electrostatic potential surface, color-coded red (−55.8 kcal/mol) to blue (55.8 kcal/mol), overlays compound ball and stick atoms (carbon, grey; hydrogen, white; nitrogen, blue; oxygen, red; and sulfur, yellow). Calculated dipole moments are depicted as arrows. B, neutral and charge transfer resonance forms, where X = C or N. See text for details.

Fig. 7. Ligand electronic difference density maps

Plots for **1** and **2** were generated at the B3LYP/6-311++G(d,p) level of theory and visualized in UCSF Chimera Alpha Version 1.5 (build 31329) with isocountour values normalized to ± 0.004 a.u. Green contours represent the accumulation of electron density in the S_1 excited state whereas red contours depict the loss of electron density from the S_0 ground state. Atom colors represent carbon (gray), hydrogen (white), nitrogen (blue), oxygen (red), and sulfur (yellow). See text for details.

Table 1

Compound Structures and Characteristics

Compound	Structure ^a	MW	λ_{max} (nm)	clogP	Volume (Å ³)
<u>Probes</u>					
ThS		493	377	-4.3	427
<u>Ligands</u>					
IMSB		554	350	3.7	418
1		310	508	4.8	277
2		312	393	4.6	285

^aThS is a mixture of substances [37]. The chemical structures of its major components are available in the PubChem Substance and Compound database through substance identifier number SID: 8137049 and/or unique chemical structure identifier CID: 415676 [52].

Table 2Calculated (cal) and experimental (exp) absorbance bands for **1** and **2**^a

Compound:	1		2	
State	λ_{cal}^b (nm)	λ_{exp} (nm)	λ_{cal}^b (nm)	λ_{exp} (nm)
S1	493 (1.51)	508	428 (1.57)	393
S2	460 (0.00)	---	330 (0.05)	---
S3	395 (0.01)	---	311 (0.04)	310

^aValues in parentheses represent calculated oscillator strengths.^bCalculated in implicit methanol solvent.